

# **Smoothing Images from Population Studies**

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# Outline

**Motivation** 

**Smoothing Strategies** 

**Multiscale Adaptive Smoothing Models** 

**Simulation Studies** 

**Real Data Analysis** 

















### **Image Registration**

Image registration is the process of transforming different sets of data into <u>one coordinate system</u>. Data may be multiple photographs, data from different sensors, from different times, or from different viewpoints.









### Image Smoothing

- Registration
- Signal-to-noise Ratio
- ♦ Gaussian
- How is it implemented?
  - Convolution with a 3D Gaussian kernel, of specified Full-width at half-maximum (FWHM) in mm



Example of Gaussian smoothing in one-dimension



The Gaussian kernel is **separable** we can smooth 2D data with two 1D convolutions.

SPM training course





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# Each voxel after smoothing effectively represents a weighted average over its local region of interest (ROI)

#### **Before convolution**



#### Convolved with a circle



#### **Gaussian convolution**





- Smoothing method is independent of data
- Degree of smoothness is arbitrary
- Effect of smoothness is profound
- The relationship between smoothing method and study design is unknown



<u>Jones et al. (2006),</u> <u>Yue et al. (2010)</u>





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What is image? an exact replica of the contents of a storage device





an optically formed duplicate or other reproduction of an object

Google/wiki



Mathematics.





Image is the point or set of points in the range corresponding to a designated point in the domain of a given function.

 $\Delta \text{ is a compact set.} \quad \tilde{x} \in \Omega \subseteq R^k$ 

 $\longrightarrow f(\tilde{x}) \in M \subseteq R^m \qquad f: \Omega \to M \subseteq R^m$ 





**Digitized Images** 

$$f: \Omega_0 \rightarrow \{0, 1, \cdots, M_0\}$$

- Sampling (grid points)  $\Omega_0 \!\in\! \Omega$
- Sampling Rate
- Quantization

 $0, 1, 2, \dots, 2^m$  for  $m = 5 \sim 12$ , that is  $M_0 = 2^m$ 



### **Image Degradation/Restoration Process**

The goal of image restoration is to improve a degrade image in some predefined sense. Schematically this process can be visualized as

$$g(x, y) = h(f(x, y)) + \eta(x, y)$$



where f is the original image, g is a degraded/noisy version of the original image and  $\tilde{f}$  is a restored version.



### **Methods**

- Filters
  - Lowpass filtering, Wiener filters, Median filtering
- Wavelet Shrinkage Denoising
  Soft and Hard thresholding
- Variational Denoising based on Bounded Variation Models
- Nonlinear Diffusion and Scale-space theory
- Bayesian Models
  Markov random field

### Issues:

- Noise Distribution
- Window Size
- Localization
- Tuning Parameters

Chen and Shen (2005)



- An image may be 'dirty' with dots, speckles, stains
- Noise removal
  - Dots can be modeled as impulses (salt-and-pepper or speckle) or continuously varying (Gaussian noise)
  - Low-pass filtering
- Problem with low-pass filtering
  - May blur edges
  - Adaptive, edge preserving











original image



1px median filter

#### **Bandwidth Selection**





3px median filter



#### 10px median filter

#### **Different Smoothing Methods**



#### **Location Adaptation**

#### **Different Smoothing Methods**



Figure Plot (a): The noisy test image. Plots (b)-(h): the reconstructed images by the local median smoothing procedure, the DWT procedure, the MRF procedure, the AWS procedure, and procedures (6)-(8), respectively.

#### Qiu (2005)







### **Propogation-Seperation Method**

Noisy image sigma=0.4



**Reconstruction local constant PS** 







Maximum Overlap DWT

nonadaptive kernel smoothing



#### **Features**

**Increasing Bandwidth** •



- **Adaptive Weights** •
- **Adaptive Estimates**



### **Propogation-Seperation Theory**

• Exponential Family  $Y(d) \sim EF(\theta(d))$  $\hat{\theta}(d) = \operatorname{argmax}_{\theta(d)} \sum_{d'} w(d, d') \ell(Y(d'), \theta(d)) = \operatorname{argmax}_{\theta(d)} \ell(\sum_{d'} \tilde{w}(d, d') Y(d'), \theta(d))$ <u>Smoothing Imaging Intensities</u>

Under strong conditions,

Katkovnik,V and Spkoiny, V. (2008) J. Polzehl and V. Spokoiny, (2005)

 $P(K(\hat{\theta}(d), \theta(d))^{1/2} > C(\log(N(D)) / N(D))^{1/(2+c)}) \rightarrow 0$ 



#### Images from Multiple Subjects Multiple Images from a single subject



Tabelow et al. (2006, 2008a, 2008b), Polzehl, et al. (2010)

- Denoising fMRI, DTI
- SPM

$$Y_i(d) = x_i^T \beta(d) + \varepsilon_i(d)\sigma(d)$$



#### **Images from Multiple Subjects**



#### **Questions of Interest**

- Complex design
  Longitudinal, Twin, and family studies
- Models with parametric and/or nonparametric components
- Consistency results
- Standard deviation images
- Testing theory

# Multiscale Adaptive Smoothing Models

My goal is to develop a class of MASMs with necessary statistical properties for imaging data collected from cross-sectional, longitudinal, twin, and familial studies.



 $= g(x, \theta(d), f(d)) \oplus \varepsilon$  $x \in R^{k}, \theta(d) \in \Theta \subset R^{p}, f(d) \in F$  $g: R^{k} \times R^{p} \times F \to M$ Problems of interest:

$$\{(\theta(d), f(d)) : d \in D\}$$
$$\{\varepsilon(d) : d \in D\}$$



### MARM

### **Multiscale Adaptive Regression Models**

- Integrate Parametric Models with PS
- Standard Deviation Image
- Consistency and Asymptotic Distribution



### **Multiscale Adaptive Regression Model**







### **Multiscale Adaptive Regression Model**

#### Identifying homogeneous regions

 $D_k$ 



Drawing a sphere with radius r0 at each voxel

Calculating the similarities between the current voxel and its neighboring voxels.





### **Model Specification**

$$\ell(\{Y_i(d'): d' \in B(d, r_0)\} \mid x_i) = \sum_{d' \in B(d, r_0)} w(d, d'; r_0) \ell(Y_i(d') \mid x_i, \theta(d))$$

 $\omega(d,d';r_0)$  is a weight function for characterizing the similarity between the data in voxels d and d'.

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### **Multiscale Adaptive Regression Model**

#### **Being Hierarchical**



Drawing nested spheres with increasing radiuses at each voxel

$$h_0 = 0 < h_1 < \dots < h_S = r_0$$





#### Being Adaptive

Sequentially determine  $\omega(d,d';h)$  and adaptively updat $\hat{m{ heta}}(d,h)$ 
















**Ø** 



MARM/PS

Learning Voxel Feature

Local Feature Adaptation

**Adaptive Estimation and Testing** 

**Automatic Stop** 



#### **Local Feature Adaptation**

• For any radius  $h_s > h_0$ , define

$$\omega(d,d';h_s) = K_{loc}(||d-d'||_2/h_s)K_{st}(D_{\theta}(d,d';h_{s-1})/C_n)$$

- $K_{loc}(u)$  and  $K_{st}(u)$  are two decreasing kernel functions
- Smoothing kernel:  $K_{loc}(u) = (1 u^2)_+$
- Similarity kernel:  $K_{st}(u) = \exp(-u)\mathbf{1}\left(u \le \frac{s+2}{s(\log s+2)}\right)$
- Dissimilarity measure:

$$egin{aligned} D_{m{ heta}}(d,d';h_{s-1}) = \ [\hat{m{ heta}}(d;h_{s-1}) - \hat{m{ heta}}(d';h_{s-1})]^T \hat{\Sigma}(\hat{m{ heta}}(d;h_{s-1}))^{-1} [\hat{m{ heta}}(d;h_{s-1}) - \hat{m{ heta}}(d';h_{s-1})]. \end{aligned}$$



### **Adaptive Estimation and Testing**

### Weighted quasi-likelihood

$$\ell_n(\boldsymbol{\theta}(d); h, \tilde{\boldsymbol{\omega}}) = \sum_{i=1}^n \sum_{d' \in B(d,h)} \tilde{\boldsymbol{\omega}}(d, d'; h) \log p(Y_i(d') | \mathbf{x}_i, \boldsymbol{\theta}(d))$$

MWQLE

$$\hat{\boldsymbol{\theta}}(d,h) = \operatorname{argmax}_{\boldsymbol{\theta}(d)} n^{-1} \ell_n(\boldsymbol{\theta}(d);h,\tilde{\boldsymbol{\omega}})$$

### Newton-Raphson Algorithm

$$\hat{\boldsymbol{\theta}}(d,h)^{(t+1)} = \hat{\boldsymbol{\theta}}(d,h)^{(t)} + \{-\partial_{\boldsymbol{\theta}(d)}^2 \ell_n(\hat{\boldsymbol{\theta}}(d,h)^{(t)};h,\tilde{\boldsymbol{\omega}})\}^{-1} \partial_{\boldsymbol{\theta}(d)} \ell_n(\hat{\boldsymbol{\theta}}(d,h)^{(t)};h,\tilde{\boldsymbol{\omega}})\}^{-1} \partial_{\boldsymbol{\theta}(d)} \ell_n(\hat{\boldsymbol{\theta}}(d,h)^{(t)};h,\tilde{\boldsymbol{\omega}})\}^{-1} \partial_{\boldsymbol{\theta}(d)} \ell_n(\hat{\boldsymbol{\theta}}(d,h)^{(t)};h,\tilde{\boldsymbol{\omega}})$$

**Expectation-Maximization Algorithm** 



### Adaptive Estimation and Testing

**Sandwich Estimator** 

$$\begin{aligned} \operatorname{Cov}[\hat{\boldsymbol{\theta}}(d,h)] &\approx \Sigma_n(\hat{\boldsymbol{\theta}}(d,h)) = [\Sigma_{n,1}(\hat{\boldsymbol{\theta}}(d,h))]^{-1} \Sigma_{n,2}(\hat{\boldsymbol{\theta}}(d,h)) [\Sigma_{n,1}(\hat{\boldsymbol{\theta}}(d,h))]^{-1} \\ \Sigma_{n,1}(\boldsymbol{\theta}(d)) &= -\partial_{\boldsymbol{\theta}(d)}^2 \ell_n(\boldsymbol{\theta}(d);h,\tilde{\boldsymbol{\omega}}) \text{ and} \\ \Sigma_{n,2}(\boldsymbol{\theta}(d)) &= \sum_{i=1}^n [\sum_{d' \in B(d,h)} \tilde{\boldsymbol{\omega}}(d,d';h) \partial_{\boldsymbol{\theta}(d)} \log p(Y_i(d')|\mathbf{x}_i,\boldsymbol{\theta}(d))]^{\otimes 2} \end{aligned}$$
Wald Test Statistic

 $[R(\hat{\boldsymbol{\theta}}(d;h)) - \mathbf{b}_0]^T [\partial_{\boldsymbol{\theta}(d)} R(\hat{\boldsymbol{\theta}}(d;h)) \hat{\Sigma}_n(\hat{\boldsymbol{\theta}}(d;h)) \partial_{\boldsymbol{\theta}(d)} R(\hat{\boldsymbol{\theta}}(d;h))^T]^{-1} [R(\hat{\boldsymbol{\theta}}(d;h)) - \mathbf{b}_0]$ 



log(Voxel size)<<Cn << sample size</pre>

**Kernel functions** 

**Conditions for M-estimators hold uniformly** 

Weak Consistency

**Asymptotical Normality** 

Asymptotically Chi-squared distribution



## **Real Data**

- Early Brain Development Project
- **Objective:** We want to assess the brain structural connectivity change in the early brain development.
- Subject: 250 infants.
- PI: John Gilmore
- MRIs: DWI, resting fMRI, and T1 MRI were acquired for each subject at 2 weeks, 1, 2, 3, 4 years old.



2 weeks 1 year 2 year Knickmeyer RC, *et al.* (2008) *J Neurosci* 28: 12176-12182.





## Infant Brain Development Data

- **Objective:** We want to assess the brain structure change in the early brain development.
- Subject: 38 infants.
- Image: Diffusion-weighted images and T1 weighted images were acquired for each subject at 2 weeks, 1 and 2 years old.
- Method: Voxel-wise imaging analysis and MARM.



### **Time Effect and Comparison**









- ACE/ADE Models
- Two-stage MARM
- Consistency and Asymptotic Distribution









At specific voxel v, we consider the structural equation model:

$$y_{ij}(v) = x_{ij}^T \beta(v) + a_{ij}(v) + d_{ij}(v) + c_i(v) + e_{ij}(v)$$

 $a_{ij}(v), d_{ij}(v), c_i(v)$  and  $e_{ij}(v)$ : the additive genetic, dominance genetic, common environmental and residual effects on i-th twin pair. We assume they are independently normally distributed with mean 0 and variance  $\sigma_a(v)^2, \sigma_d(v)^2, \sigma_c(v)^2$  and  $\sigma_e(v)^2$ .





There are two sets of parameters: mean structure variance structure

 $\omega(d,d';h_s) = K_{loc}(||d-d'||_2/h_s)K_{st}(D_{\theta}(d,d';h_{s-1})/C_n)$ 

 $D_{\theta}(d,d';h_{s-1}) = \\ [\hat{\theta}(d;h_{s-1}) - \hat{\theta}(d';h_{s-1})]^T \hat{\Sigma}(\hat{\theta}(d;h_{s-1}))^{-1} [\hat{\theta}(d;h_{s-1}) - \hat{\theta}(d';h_{s-1})].$ 

Question of interest: Mean and variance images may have different patterns.

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### **Two-stage Approach**

Mean structure

$$Y_{ij}(d) = x_{ij}^T \beta(d) + \varepsilon_{ij}(d) \Rightarrow \{\hat{\beta}(d,h) : d \in D\}$$

Variance structure

$$\{Y_{ij}(d) - x_{ij}^T \hat{\beta}(d;h)\}^2 = z_{ij}^T \rho(d) + \delta_{ij}(d) \Longrightarrow \{\hat{\rho}(d;h) : d \in D\}$$





# It is dangerous to use Gaussian-kernel to smooth imaging data and then carry out twin analysis.



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### Multiscale Adaptive Smoothing Models for HRF in fMRI

- Convolution Models in Frequency Domain
- Back Fitting Methods
- Multi-stage MARM



## **Multiscale Adaptive Smoothing Model**

### D: 3D volume

 $N_D$ : the number of points on D

d: a voxel in D

 $\{Y(t,d): t = 1 \times t_{TR}, \dots, T \times t_{TR}, d \in D\}: \text{ spatial-temporal process}$  $\{X(t): t \in [0, T \times t_{TR}]\}: \text{ external stimulus process}$  $\{H(t,d): t \in [0, T \times t_{TR}], d \in D\}: \text{ spatial-temporal HRF process}$  $\{\varepsilon(t,d): t \in [0, T \times t_{TR}], d \in D\}: \text{ error process}$ 



## **Voxel-wise Approach**

$$Y(t,d) = H(\bullet,d) \otimes X(t) + \varepsilon(t,d) = \int H(t-u,d)X(u)du + \varepsilon(t,d)$$
  
**time-domain**  

$$H(t,d) = \sum_{k=1}^{K} \beta_k(d)f_k(t)$$
  

$$Y(t,d) = \sum_{k=1}^{K} \beta_k(d)\int f_k(t-u,d)X(u)du + \varepsilon(t,d) = \sum_{k=1}^{K} \beta_k(d)x_k(t) + \varepsilon(t,d)$$

### frequency-domain

$$F_{Y}(f,d) = F_{H}(f,d)F_{X}(f) + F_{\varepsilon}(t,d) \text{ for } f \in [0, T \times t_{TR}]$$
  
$$F_{Y}(t,d) = \int_{0}^{T \times t_{TR}} Y(t,d) \exp(-2\pi i f t/(T \times t_{TR})) dt$$



### Continuous

$$F_Y(f,d) = F_H(f,d)F_X(f) + F_\varepsilon(t,d) \text{ for } f \in [0, T \times t_{TR}]$$

### Discrete

$$\phi_Y(f,d) = \phi_H(f,d)\phi_X(f) + \phi_\varepsilon(f,d) \text{ for } f \in [0, T \times t_{TR}]$$

$$\phi_Y(f,d) = \sum_{t=0}^{T \times t_{TR}} Y(t,d) \exp(-2\pi i f t / (T \times t_{TR}))$$

### **Key Assumptions:**

$$\phi_{\varepsilon}(f,d) \sim (0,1(f=f)\sigma(f,f;d,d))$$

 $\phi_H(f,d)$  is piecewisely smooth for  $(f,d) \in N(f,d)$ 









$$\phi_Y(f,d) = \phi_H(f,d)\phi_X(f) + \phi_\varepsilon(f,d) \text{ for } (f,d) \in \mathcal{N}(f,d)$$

### **Approximation**

 $\phi_Y(f_k, d') = \phi_H(f_k, d')\phi_X(f_k) + \phi_\varepsilon(f_k, d')$  $\approx \phi_H(f, d)\phi_X(f_k) + \phi_\varepsilon(f_k, d')$ 

$$(f_k, d') \in B((f, d); \varepsilon, r) = (f - \varepsilon, f + \varepsilon) \times B(d', r)$$

### **Multiple Events: Backfitting Methods**

Unknown



### Weighted LSE

$$L(\phi_{H}(f,d);B((f,d);r,h)) = \sum_{(f_{k},d')} [\phi_{Y}(f_{k},d') - \phi_{H}(f,d)\phi_{X}(f_{k})]^{2} w(f,d,f_{k},d';\varepsilon,r)$$

$$\hat{\phi}_{H}(f,d) = \sum_{(f_{k},d)} \phi_{Y}(f_{k},d) \overline{\phi}_{X}(f_{k}) w(f,d,f_{k},d;\varepsilon,r) / \sum_{(f_{k},d)} \phi_{X}(f_{k}) \overline{\phi}_{X}(f_{k}) w(f,d,f_{k},d;\varepsilon,r)$$

$$Vor(\hat{\phi}_{X}(f_{k},d))$$

 $\operatorname{Var}(\phi_H(f, d))$ 

### **Estimated HRF**

$$\hat{H}(t,d) = \sum_{k=0}^{T-1} \hat{\phi}_{H}(f,d) \exp(i2\pi t f_{k}) [1 - \cos(2\pi t/T)] / (2\pi^{2} t^{2}/T)$$



## **Simulation II: Multivariate Case**

The background image and the simulated one with their related curves. In this simulation the smallest SNR is between 0.5 and 0.7.



Three activated regions for each sequence of events correspond with three different HRFs:  $h_i(t)/2$ ,  $h_i(t)/4$ ,  $h_i(t)/6$ , j=1,2,3

$$\begin{aligned} h_j(t) &= A_j \cdot (t/d_{j1})^{a_{j1}} \exp\left(-(t-d_{j1})/b_{j1}\right) - c(t/d_{j2})^{a_{j2}} \exp\left(-(t-d_{j2})/b_{j2}\right) & j = 1, 2, 3\\ \epsilon(t) &\sim N(0, \sigma^2) & X_j(t) \sim B(1, 0.15) \end{aligned}$$



## The estimates of the HRFs, from the left to right, are the 1st, 2nd and 3rd sequences of events.





## Comparison with Lindquist et al (2009)

 $D = \frac{1}{n} \frac{1}{m} \sum_{i=1}^{n} \sum_{j=1}^{m} (|\hat{x}_{ij} - x_0| - |\hat{y}_{ij} - x_0|)$  n is the sample size, m is the number of voxels in each active region.

Param		sFIR				IR				GAM			
Н		A1	A2	A3		A1	A2	A3		A1	A2	A3	
	CI	-0.02	-0.04	-0.09	C1	-0.11	-0.16	-0.32	C1	-0.13	-0.20	-0.42	
	U1	(0.045)	(0.045)	(0.060)		(0.0819)	(0.115)	(0.218)		(0.039)	(0.044)	(0.059)	
	CO	-0.02	-0.04	-0.10	Co	-0.09	-0.14	-0.27	C2	-0.11	-0.17	-0.36	
	04	(0.041)	(0.043)	(0.057)	02	(0.0699)	(0.096)	(0.175)		(0.041)	(0.045)	(0.057)	
	C 2	-0.01	-0.02	-0.07	C3	-0.07	-0.10	-0.21	C3	-0.07	-0.11	-0.25	
	U3	(0.046)	(0.047)	(0.064)		(0.0673)	(0.089)	(0.161)		(0.038)	(0.045)	(0.066)	
т		A1	A2	A3	Γ	A1	A2	A3		A1	A2	A3	
	C1	-0.08	0.05	0.01	CI	-3.74	-3.49	-3.19	C1	-2.50	-2.66	-2.84	
		(0.722)	(0.326)	(0.073)	0	(3.313)	(3.309)	(3.292)		(0.425)	(0.298)	(0.070)	
	0	-0.05	0.07	0.01	C	-3.50	-3.34	-2.88	C2	-2.57	-2.75	-2.91	
	04	(0.685)	(0.292)	(0.069)	0	(3.440)	(3.475)	(3.419)		(0.452)	(0.287)	(0.069)	
	C2	-0.55	-0.10	-0.10	CO	-3.54	-3.26	-3.03	C3	-2.46	-2.66	-2.87	
	U3	(1.159)	(0.513)	(0.513)	0.	(3.404)	(3.430)	(3.415)		(0.577)	(0.427)	(0.254)	
w		A1	A2	A3		A1	A2	A3		A1	A2	A3	
	C1	-0.20	-0.28	-0.42	C1	-1.70	-1.73	-1.66	C1	-3.33	-3.41	-3.46	
		(0.671)	(0.596)	(0.518)		(2.122)	(2.127)	(2.094)		(0.623)	(0.576)	(0.515)	
	CO	-0.38	-0.41	-0.49	C2	-1.78	-1.80	-1.79	C2	-3.35	-3.41	-3.49	
	04	(0.760)	(0.597)	(0.513)		(2.143)	(2.099)	(2.018)		(0.634)	(0.575)	(0.512)	
	C3	-0.32	-0.33	-0.48	C3	-1.79	-1.85	-2.08	C3	-3.30	-3.42	-3.63	
		(0.870)	(0.741)	(0.658)		(2.179)	(2.123)	(2.221)		(0.713)	(0.677)	(0.550)	

Comparisons of the differences of the absolute errors between our method with smooth finite impulse response (sFIR), inverse logit (IL) and SPM canonical HRF (GAM), respectively. C1, C2 and C3 denotes the 1st, 2nd and 3rdsequences of events, respectively. A1, A2 and A3 denotes the1st, 2nd and 3rd active regions. Values in the blanket are the standard deviations. H=Height, W=Width, T=Time-to-Peak.



This data set is from a memory related experiment to compare the neural correlates of relational memory during implicit (nonstrategic) versus explicit (conscious, strategic) retrieval.

There are four different sequences of stimuli.

We use SPM8 to preprocess the images including the realignment, timing slicing, segmentation, coregistration, normalization and spatial smoothing.



We focus on some significant regions of interest (ROI) detected by SPM to study the HRFs of the voxels by our method. The results are verified by sFIR and GAM.







(1)-(4) Estimated HRFs at the significant ROIs corresponding each condition from MASM (red), sFIR(green) and GAM(yellow); (5)-(8) Estimated HRFs from only MASM in the each ROI.


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Society of Imaging Neuroscience Statisticians (SINS)

http://www.mscs.mu.edu/~dbrowe/sins.html

Roundtables in ENAR 2011 and JSM 2011.









$(d) \qquad 0.0 \qquad 0.2 \qquad 0.4 \qquad 0.6 \qquad 0.8$	
--	--

red

yellow

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white



	$\chi^2(3) - 3$							N(0, 1)						
		n = 60				n = 80			n = 60			n = 80		
$\beta_2(d)$		$h_0$	$h_5$	$h_{10}$	$h_0$	$h_5$	$h_{10}$	$h_0$	$h_5$	$h_{10}$	$h_0$	$h_5$	$h_{10}$	
0.0	BIAS	0.00	0.00	0.01	0.00	0.00	0.00	0.00	0.00	0.00	0.00	0.00	0.00	
	RMS	0.48	0.35	0.26	0.41	0.31	0.22	0.20	0.15	0.11	0.17	0.13	0.09	
	SD	0.47	0.34	0.24	0.41	0.30	0.21	0.19	0.14	0.10	0.17	0.12	0.09	
	RE	1.03	1.05	1.06	1.02	1.03	1.04	1.03	1.05	1.06	1.02	1.03	1.04	
0.2	BIAS	0.00	-0.03	-0.07	0.01	-0.02	-0.06	0.00	-0.03	-0.05	0.00	-0.02	-0.05	
	RMS	0.46	0.34	0.24	0.39	0.29	0.21	0.19	0.14	0.11	0.16	0.12	0.09	
	SD	0.46	0.33	0.24	0.40	0.29	0.21	0.19	0.14	0.10	0.16	0.12	0.09	
	RE	1.01	1.01	1.01	0.99	1.00	1.01	1.02	1.04	1.06	1.02	1.02	1.03	
0.4	BIAS	-0.01	-0.05	-0.09	0.01	-0.02	-0.06	0.00	0.00	-0.01	0.00	0.00	0.00	
	RMS	0.46	0.34	0.25	0.40	0.30	0.22	0.19	0.15	0.12	0.16	0.13	0.10	
	SD	0.46	0.33	0.24	0.40	0.29	0.21	0.19	0.14	0.11	0.16	0.12	0.09	
	RE	1.01	1.02	1.03	1.01	1.02	1.03	1.03	1.05	1.07	1.00	1.01	1.02	
0.6	BIAS	0.00	-0.05	-0.09	0.00	-0.04	-0.07	0.00	0.01	0.02	0.00	0.00	0.01	
	RMS	0.46	0.35	0.26	0.40	0.30	0.23	0.19	0.15	0.12	0.16	0.13	0.10	
	SD	0.46	0.34	0.25	0.40	0.30	0.22	0.19	0.14	0.11	0.16	0.13	0.10	
	RE	1.01	1.03	1.04	1.01	1.02	1.03	1.02	1.04	1.06	1.01	1.03	1.04	
0.8	BIAS	0.00	-0.04	-0.06	0.00	-0.02	-0.05	0.00	-0.01	-0.02	0.00	0.00	-0.01	
	RMS	0.47	0.35	0.26	0.40	0.30	0.23	0.19	0.15	0.11	0.17	0.13	0.10	
	SD	0.46	0.34	0.25	0.40	0.30	0.22	0.19	0.14	0.11	0.16	0.12	0.09	
	RE	1.02	1.03	1.04	1.01	1.02	1.03	1.02	1.04	1.05	1.03	1.05	1.06	





$$\hat{\beta}_3(d,h_{10})$$

















**Table 2.** Simulation study for  $W_{\mu}(d, h)$ : estimates (ES) and standard errors (SE) of rejection rates for pixels inside the five ROIs were reported at 2 different scales  $(h_0, h_{10})$ , 2 different distributions  $(N(0, 1) \text{ and } \chi^2(3) - 3)$ , and 2 different sample sizes (n = 60, 80) at  $\alpha = 5\%$ . For each case, 1,000 simulated data sets were used.

			N(0	), 1)		$\chi^2(3) - 3$				
		<i>n</i> =	= 60	<i>n</i> =	= 80	<i>n</i> =	= 60	n = 80		
$\beta_2(d)$	s	ES	SE	ES	SE	ES	SE	ES	SE	
0.2	$h_0$	0.20	0.066	0.24	0.070	0.08	0.038	0.08	0.037	
	$h_{10}$	0.30	0.126	0.38	0.121	0.10	0.069	0.18	0.081	
0.4	$h_0$	0.56	0.090	0.67	0.079	0.15	0.065	0.18	0.070	
	$h_{10}$	0.93	0.051	0.98	0.030	0.26	0.129	0.35	0.159	
0.6	$h_0$	0.88	0.039	0.95	0.024	0.27	0.057	0.33	0.050	
	$h_{10}$	1.00	0.004	1.00	0.004	0.51	0.091	0.63	0.083	
0.8	$h_0$	0.99	0.015	1.00	0.005	0.43	0.080	0.52	0.080	
	$h_{10}$	0.99	0.010	0.99	0.011	0.78	0.099	0.90	0.006	
0.0	$h_0$	0.07	0.006	0.07	0.006	0.06	0.007	0.07	0.006	
	$h_{10}$	0.08	0.011	0.07	0.011	0.07	0.012	0.08	0.012	



## **Early Brain Development: Structural connectivity**

#### **Comparison:**

#### MAGEEC(0) versus MAGEEC(5)



#### **Model Selection:**

