# Application of Potential Theory to MR Elastography

Dr. Corina S. Drapaca

cdrapaca@math.uwaterloo.ca

Department of Applied Mathematics
University of Waterloo

Waterloo, ON, N2L 3G1 Canada

Work done in collaboration with Dr.R. Ehman, Dr.A. Manduca and the MRE Lab Mayo Clinic, College of Medicine, Rochester, MN, USA

Problem: Finding material parameters of biological materials in vivo and map them in an anatomically meaningful image that provides useful clinical information (elastogram).

Problem: Finding material parameters of biological materials in vivo and map them in an anatomically meaningful image that provides useful clinical information (elastogram).

Applications: Diagnostic tool in finding tumors and other diseases (tumors tend to be harder than the surrounding normal tissue) (elastography = 'palpation by imaging'), trauma and surgical simulations.

Problem: Finding material parameters of biological materials in vivo and map them in an anatomically meaningful image that provides useful clinical information (elastogram).

Applications: Diagnostic tool in finding tumors and other diseases (tumors tend to be harder than the surrounding normal tissue) (elastography = 'palpation by imaging'), trauma and surgical simulations.

In particular: any mathematical model capable to predict the response of the brain to internal (hydrocephalus) or external (trauma) forces requires accurate stiffness and attenuation values of the brain.

Problem: Finding material parameters of biological materials in vivo and map them in an anatomically meaningful image that provides useful clinical information (elastogram).

Applications: Diagnostic tool in finding tumors and other diseases (tumors tend to be harder than the surrounding normal tissue) (elastography = 'palpation by imaging'), trauma and surgical simulations.

In particular: any mathematical model capable to predict the response of the brain to internal (hydrocephalus) or external (trauma) forces requires accurate stiffness and attenuation values of the brain.

### Imaging modalities:

- ultrasound (sonoelastography or sonoelasticity).
- MRI (magnetic resonance elastography).
- optics (optical elastography).

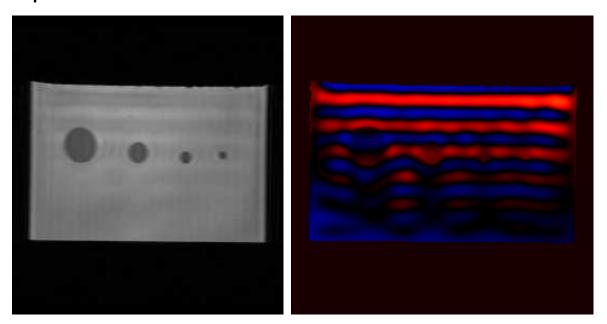
- We can employ different tissue excitations:
  - the tissue is compressed (static elastography) (Ophir et al. 1991, Cespedes et al. 1993, Krouskop et al. 1998).
  - a time harmonic excitation made on the boundary creates a time harmonic wave in the tissue (dynamic elastography)
     (Muthupillai et al. 1995, Lorenzen et al. 2003, Sinkus et al. 2000, Plewes et al. 2000, McKnight et al. 2002, Dresner et al. 2001).
  - a time dependent pulse on the boundary creates a propagating wave in the tissue (transient elastography) (Catheline et al. 1999, Sandrin et al. 2003).
  - the use of the acoustic radiation force by focusing an ultrasound beam at a chosen location (remote elastography).

- We can employ different tissue excitations:
  - the tissue is compressed (static elastography) (Ophir et al. 1991, Cespedes et al. 1993, Krouskop et al. 1998).
  - a time harmonic excitation made on the boundary creates a time harmonic wave in the tissue (dynamic elastography)
     (Muthupillai et al. 1995, Lorenzen et al. 2003, Sinkus et al. 2000, Plewes et al. 2000, McKnight et al. 2002, Dresner et al. 2001).
  - a time dependent pulse on the boundary creates a propagating wave in the tissue (transient elastography) (Catheline et al. 1999, Sandrin et al. 2003).
  - the use of the acoustic radiation force by focusing an ultrasound beam at a chosen location (remote elastography).
- Image different parameters of tissue motion: strain, stress, velocity, amplitude, phase, vibration, etc.

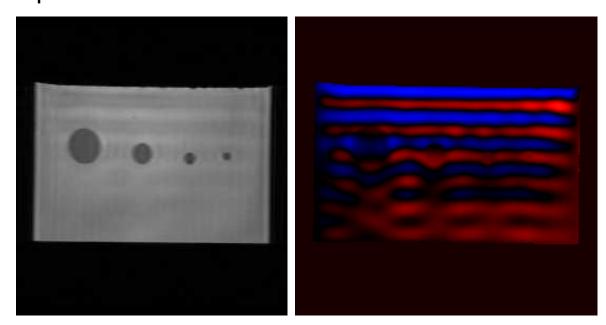
- We can employ different tissue excitations:
  - the tissue is compressed (static elastography) (Ophir et al. 1991, Cespedes et al. 1993, Krouskop et al. 1998).
  - a time harmonic excitation made on the boundary creates a time harmonic wave in the tissue (dynamic elastography)
     (Muthupillai et al. 1995, Lorenzen et al. 2003, Sinkus et al. 2000, Plewes et al. 2000, McKnight et al. 2002, Dresner et al. 2001).
  - a time dependent pulse on the boundary creates a propagating wave in the tissue (transient elastography) (Catheline et al. 1999, Sandrin et al. 2003).
  - the use of the acoustic radiation force by focusing an ultrasound beam at a chosen location (remote elastography).
- Image different parameters of tissue motion: strain, stress, velocity, amplitude, phase, vibration, etc.
- Present work: dynamic MR elastography, elastogram of the shear wave speed.

- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.

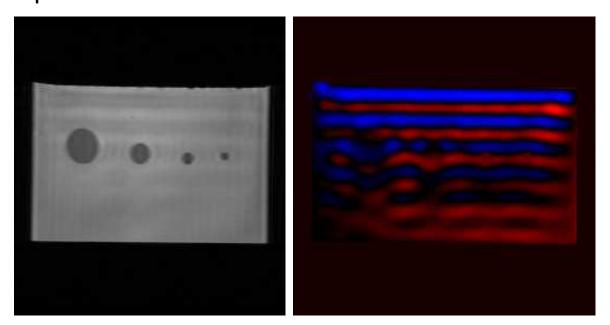
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



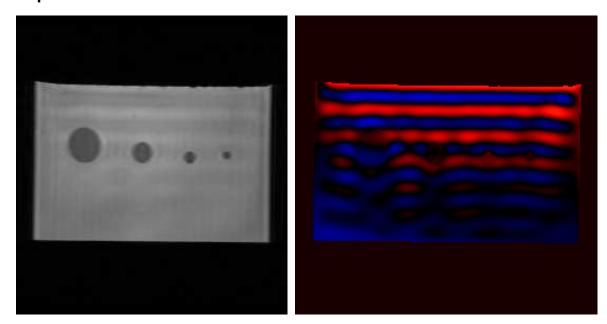
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



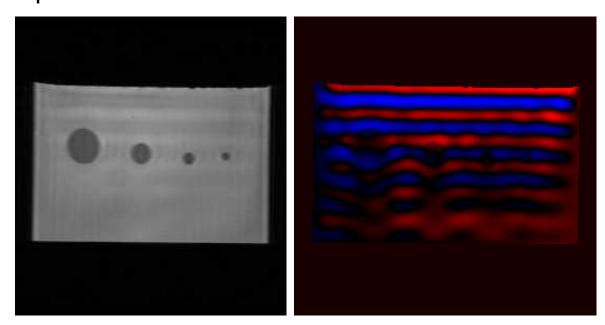
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



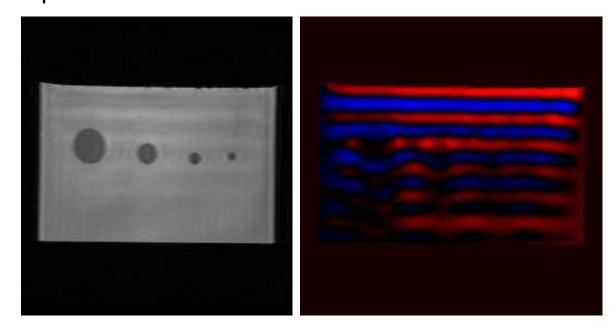
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



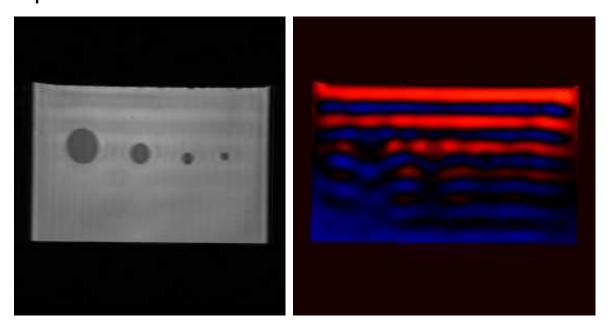
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



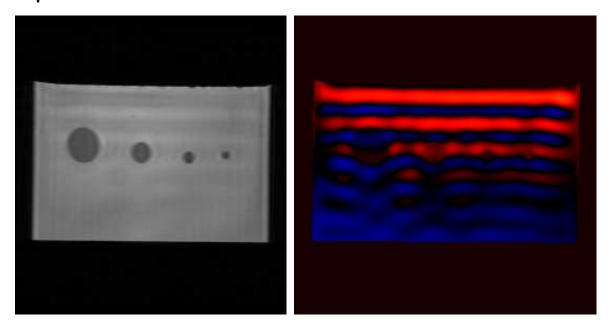
- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.



- MR images are recorded while a vibrating plate placed on the skin propagates mechanical shear waves of a known frequency in the tissue.
- From the images of the motion we estimate the wavelength of the shear wave.
- The MRI signal contains both amplitude and phase information. In the linear regime, the phase-difference field is directly proportional to the displacement field.
- Once the displacement field is known, we need a constitutive model for the biological tissues from which to extract the material parameters (the shear modulus).

Constitutive Assumptions: Biological tissues are locally homogeneous, isotropic, almost incompressible, linear viscoelastic materials of density  $\approx 1$  g/cm<sup>3</sup> (Burelew et al., 1980).

Navier equations for displacements in the frequency domain are:

$$\left(\Lambda(\omega) + M(\omega)\right) \nabla \left(\nabla \cdot \vec{U}(\vec{x}, \omega)\right) + M(\omega) \nabla^2 \vec{U}(\vec{x}, \omega) = -\omega^2 \vec{U}(\vec{x}, \omega)$$

Constitutive Assumptions: Biological tissues are locally homogeneous, isotropic, almost incompressible, linear viscoelastic materials of density  $\approx 1$  g/cm<sup>3</sup> (Burelew et al., 1980).

Navier equations for displacements in the frequency domain are:

$$\left(\Lambda(\omega) + M(\omega)\right) \nabla \left(\nabla \cdot \vec{U}(\vec{x}, \omega)\right) + M(\omega) \nabla^2 \vec{U}(\vec{x}, \omega) = -\omega^2 \vec{U}(\vec{x}, \omega)$$

• For biological tissues,  $\Lambda >> M$  ( $\Lambda = \mathcal{O}(10^9)$  Pa,  $M = \mathcal{O}(10^2 \div 10^7)$  Pa), M varies strongly with tissue pathology.

Constitutive Assumptions: Biological tissues are locally homogeneous, isotropic, almost incompressible, linear viscoelastic materials of density  $\approx 1$  g/cm<sup>3</sup> (Burelew et al., 1980).

Navier equations for displacements in the frequency domain are:

$$\left(\Lambda(\omega) + M(\omega)\right) \nabla \left(\nabla \cdot \vec{U}(\vec{x}, \omega)\right) + M(\omega) \nabla^2 \vec{U}(\vec{x}, \omega) = -\omega^2 \vec{U}(\vec{x}, \omega)$$

- For biological tissues,  $\Lambda >> M$  ( $\Lambda = \mathcal{O}(10^9)$  Pa,  $M = \mathcal{O}(10^2 \div 10^7)$  Pa), M varies strongly with tissue pathology.
- Two reduced forms of Navier equations:
  - DI equation:  $M\nabla^2 \vec{U} = -\omega^2 \vec{U}$
  - Curl-DI equation:  $M\nabla^2(\nabla \times \vec{U}) = -\omega^2(\nabla \times \vec{U})$
- *M* can be found using the method of algebraic inversion of differential equations AIDE (Oliphant et al., 2001).

Problem: longitudinal wave effects (DI equation) and higher order numerical differentiation (Curl-DI equation) can affect the AIDE stiffness values.

Problem: longitudinal wave effects (DI equation) and higher order numerical differentiation (Curl-DI equation) can affect the AIDE stiffness values.

- Use:
  - Potential theory to lower the order of numerical differentiation.
  - The curl operator to eliminate the longitudinal effects.

Problem: longitudinal wave effects (DI equation) and higher order numerical differentiation (Curl-DI equation) can affect the AIDE stiffness values.

- Use:
  - Potential theory to lower the order of numerical differentiation.
  - The curl operator to eliminate the longitudinal effects.

- Motivation comes from the Helmholtz decomposition method:
  - Allows the breakup of a vector wave field into its longitudinal and shear components.
  - One can then process only the shear component of the displacement field.
  - Mathematical proof is based on the concept of a potential vector field.

Replace the displacement field by its corresponding potential field:

$$\vec{V}(\vec{x}) = -\frac{1}{4\pi} \int \int \int \frac{1}{|\vec{x} - \vec{y}|} \vec{U}(\vec{y}) d\vec{y}$$
 (2D case)

Replace the displacement field by its corresponding potential field:

$$\vec{V}(\vec{x}) = -\frac{1}{4\pi} \int \int \int \frac{1}{|\vec{x} - \vec{y}|} \vec{U}(\vec{y}) d\vec{y}$$
 (2D case)

- The potential field satisfies the Navier equations and thus:
  - PDI equation (analogous to DI equation):

$$M\nabla^2 \vec{U} = -\omega^2 \vec{U} \Rightarrow M\vec{U} = -\omega^2 \vec{V}$$
 no derivatives

Curl-PDI equation (analogous to Curl-DI equation):

$$M\nabla^2(\nabla \times \vec{U}) = -\omega^2(\nabla \times \vec{U}) \Rightarrow M(\nabla \times \vec{U}) = -\omega^2(\nabla \times \vec{V})$$
  
only first order derivatives

Results: We compare DI and Curl-PDI.

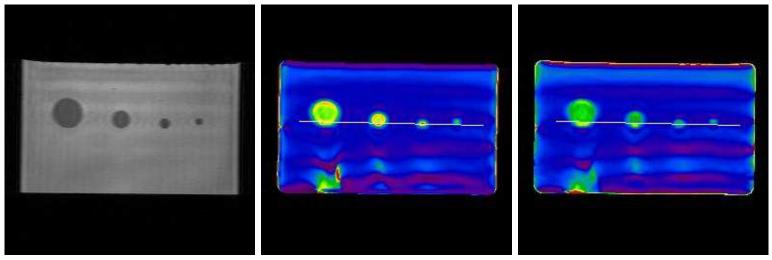
• The elastogram is made of the square of the shear wave speed values,  $c_s^2$ , where:

$$c_s(f) = \sqrt{\frac{2(Re(M)^2 + Im(M)^2)}{Re(M) + \sqrt{Re(M)^2 + Im(M)^2}}}$$

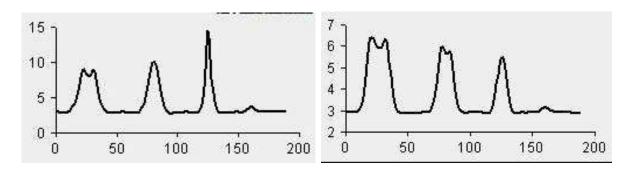
Results: We compare DI and Curl-PDI.

• The elastogram is made of the square of the shear wave speed values,  $c_s^2$ , where:

$$c_s(f) = \sqrt{\frac{2(Re(M)^2 + Im(M)^2)}{Re(M) + \sqrt{Re(M)^2 + Im(M)^2}}}$$



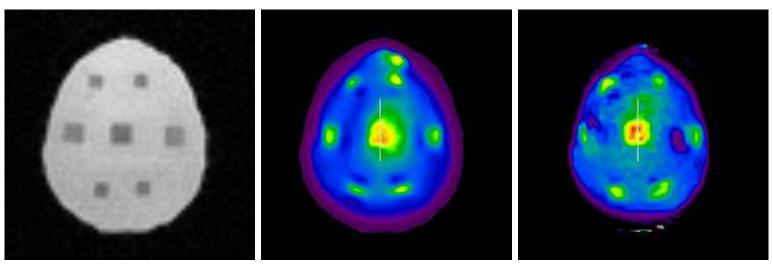
Up: Magnitude (left), DI (center), Curl-PDI (right); Down: DI values (left), Curl-PDI values (right)



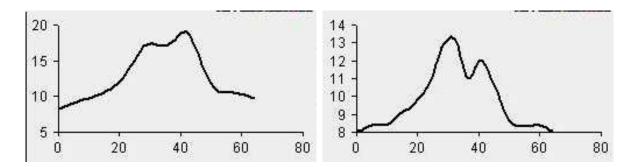
Results: We compare DI and Curl-PDI.

• The elastogram is made of the square of the shear wave speed values,  $c_s^2$ , where:

$$c_s(f) = \sqrt{\frac{2(Re(M)^2 + Im(M)^2)}{Re(M) + \sqrt{Re(M)^2 + Im(M)^2}}}$$



Up: Magnitude (left), DI (center), Curl-PDI (right); Down: DI values (left), Curl-PDI values (right)



#### Discussion:

- By using the potential of the displacement field we reduced the order of numerical differentiation:
  - the curl operator can be used;
  - more stable results (has the effect of a regularization method for the inverse problem of elastography).

#### Discussion:

- By using the potential of the displacement field we reduced the order of numerical differentiation:
  - the curl operator can be used;
  - more stable results (has the effect of a regularization method for the inverse problem of elastography).
- The anisotropy of the tissues generates quasi-longitudinal and quasi-shear waves. ⇒ Helmholtz decomposition fails ⇒ How to generalize Helmholtz method using multiscaling (fractional order) spatial derivatives?

#### Discussion:

- By using the potential of the displacement field we reduced the order of numerical differentiation:
  - the curl operator can be used;
  - more stable results (has the effect of a regularization method for the inverse problem of elastography).
- The anisotropy of the tissues generates quasi-longitudinal and quasi-shear waves. ⇒ Helmholtz decomposition fails ⇒ How to generalize Helmholtz method using multiscaling (fractional order) spatial derivatives?
- Use an appropriate constitutive model (material with microstructure, peridynamic model, non-linear material). How to model and measure residual stresses (present in the hydrocephalic brain, for example)?

#### Discussion:

- By using the potential of the displacement field we reduced the order of numerical differentiation:
  - the curl operator can be used;
  - more stable results (has the effect of a regularization method for the inverse problem of elastography).
- The anisotropy of the tissues generates quasi-longitudinal and quasi-shear waves. ⇒ Helmholtz decomposition fails ⇒ How to generalize Helmholtz method using multiscaling (fractional order) spatial derivatives?
- Use an appropriate constitutive model (material with microstructure, peridynamic model, non-linear material). How to model and measure residual stresses (present in the hydrocephalic brain, for example)?

### **THANK YOU!**