

# Cancer Growth

Tissue Level Signalling (Tumour Angiogenesis factors)  
Oxygen etc  
PDE

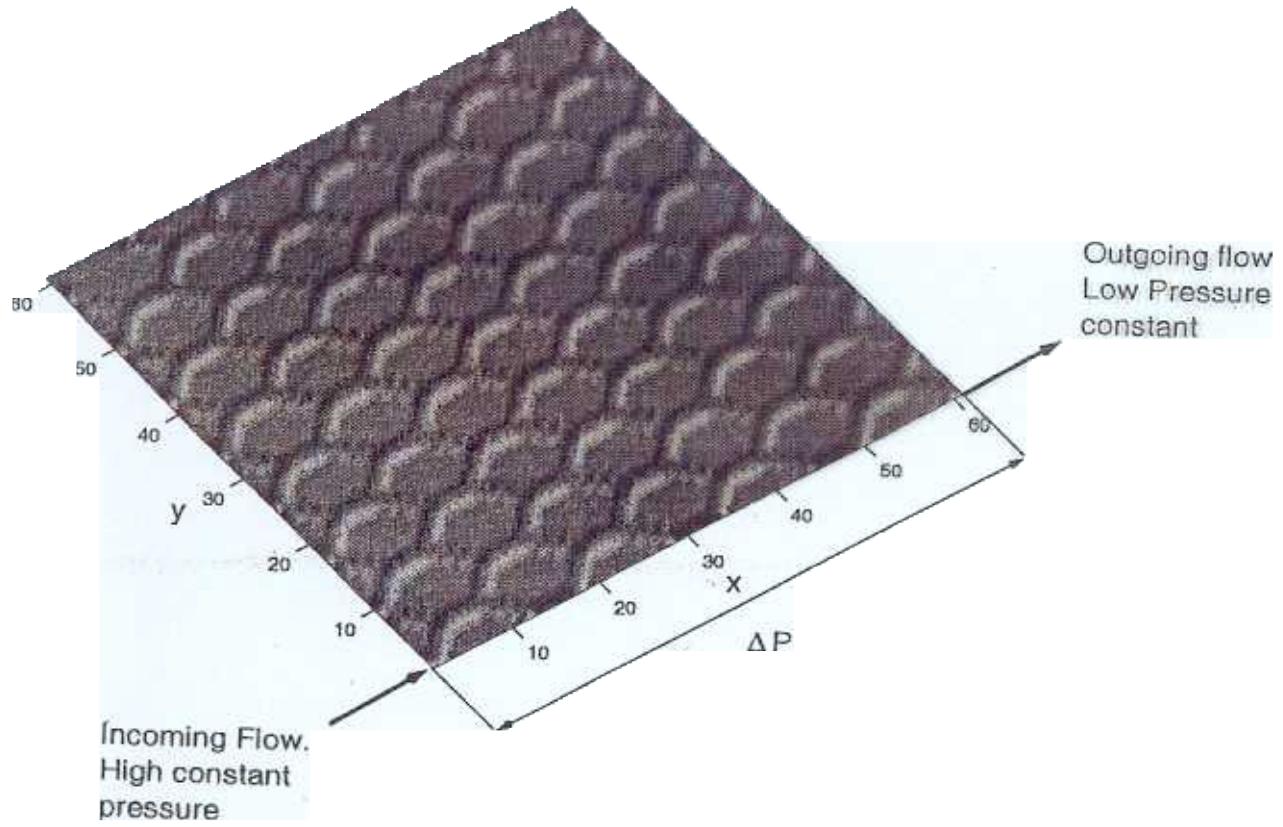
Cells

Automaton Elements

Intracellular Ce Cycle  
molecular elements

ODEs

Alfonso Byrne PKM J theor Biol 225, 257-274  
~~to appear~~ 2003  
in prep



Hexagonal network, similar to avian yolk sac (Honda & Yoshizato, 1997)

Liver

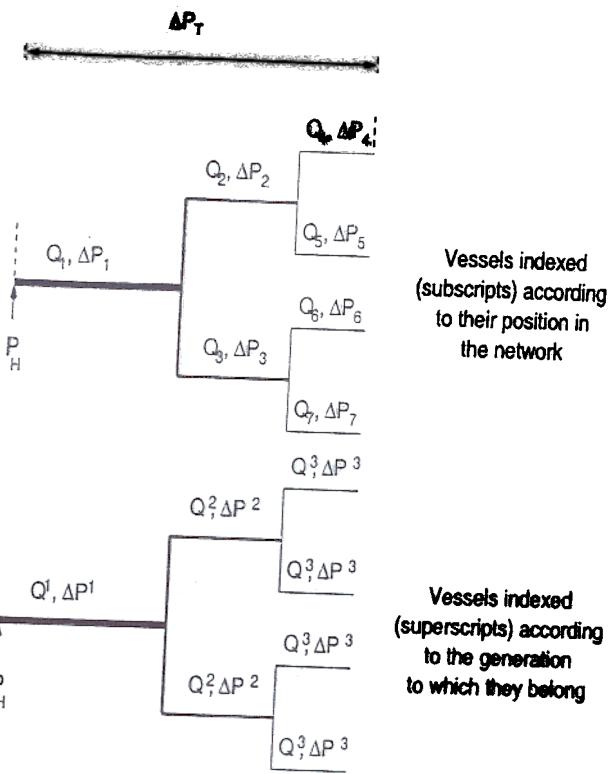


Fig. 5. Schematic representation of the branching structure used in our simulations. See text for details.

Using these results plus

$$Q_i = Q_j + Q_k \quad (\text{flow conservation at each bifurcation})$$

and

$$\sum_j \Delta P_j = \Delta P_T \quad \text{pressure drop across the whole network}$$

$$\Delta P_j = \frac{8\mu\ell(R_j)L_j}{\pi R_j^4} Q_j \quad (\text{Poiseuille flow})$$

Fahraeus -  
Lindquist  
effect

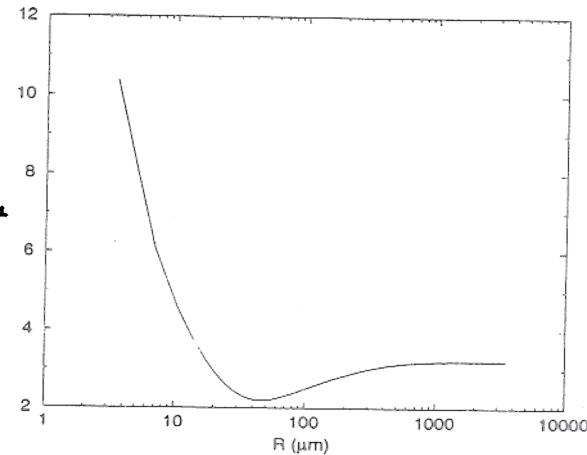


Fig. 3. Relative blood viscosity  $\mu(R)$  as a function of the radius ( $R$ ) of the vessel.

Data from [10] for a proportion of the total volume of blood occupied by red blood cells (hematocrit) of 0.45. (Pries et al., 1994)

## Blood rheology

Avg. red blood cell diameter in humans ~7.8 μm

$$\mu(R) = \left(\frac{R}{R-R_0}\right)^2 \left(1 + \left(\frac{R}{R-R_0}\right)^2 (a_0 + a_1 e^{-\lambda_1 R} - a_2 e^{-\lambda_2 R})\right)$$

Reformulate Minimization principle

$$\Rightarrow \dot{\bar{Q}} = R^3 \frac{\pi}{2\sqrt{\mu_0}} \sqrt{\frac{\alpha b}{4\mu - R\mu_R}}$$

$$R_0 = 0.55$$

$$a_0 = 2.2$$

$$a_1 = 6$$

$$a_2 = 2.4$$

$$\lambda_1 = 0.17$$

$$\lambda_2 = 0.09$$

$$\delta = 0.645$$

Numerical Soln  $\Rightarrow$

$$\dot{\bar{Q}}_i = CR^{\alpha_i}$$

$$\alpha_i = \begin{cases} 3.00 & \text{if } R_i > R_{cr1} \\ 2.87 & \text{if } R_{cr2} < R_i < R_{cr1} \\ 3.66 & \text{if } R_i < R_{cr2} \end{cases}$$

$$R_{cr1} \approx 270 \mu\text{m}$$

$$R_{cr2} \approx 45 \mu\text{m}$$

$$C_i = \text{etc.}$$

## Tumour Growth

First work out distribution of  $O_2$  (nutrient)

To do so must consider vasculature metabolic response

$$R(t+dt) = R(t) + R \Delta t \left( \ln \left( \frac{T_w}{T(P)} \right) + k_m \ln \left( \frac{Q_{ref}}{Q_H} \right) \right)$$

$R$  radius

$Q$  flow rate

haematocrit

WSS

$P$  pressure (transmural)

response to  
mechanical  
stimulus

shrinkage  $\sim k_s$   
(Pries et al 1988)

$$T(P) = 100 - 86 \exp(-5000 \ln(\ln P))^{5/3} \quad (\text{at mesentery})$$

\* Haematocrit  $\mu$   $\mu(H, R)$  Pries et al 1994  $\mu \uparrow$  with  $H$ )

\* At a bifurcation

$$H_p = H_1 + H_2$$

$$\frac{H_1}{H_2} \propto \frac{v_1}{v_2} \text{ if } \frac{v_1}{v_2} < T \quad (\text{Fung 993})$$

$$H_p \text{ if } \frac{v_1}{v_2} > T$$

## Algorithm for structural adaptation

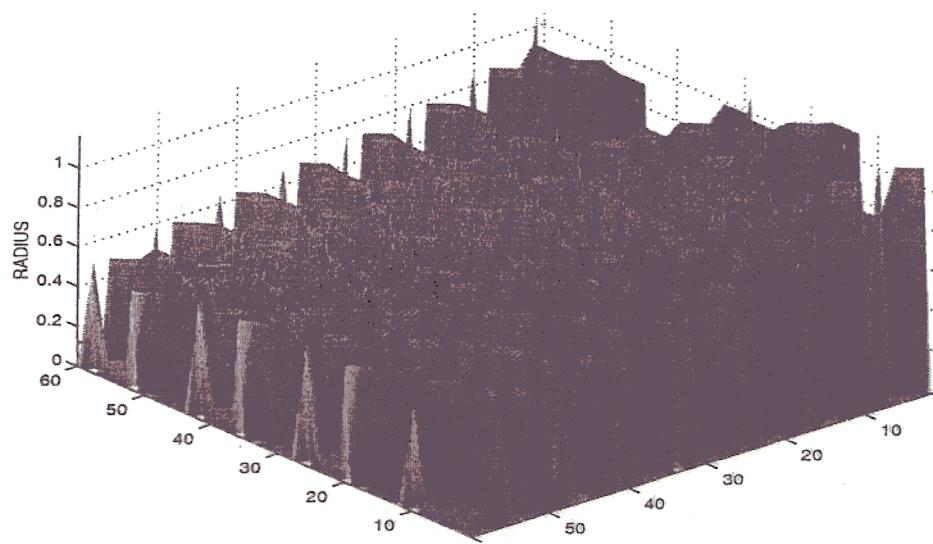
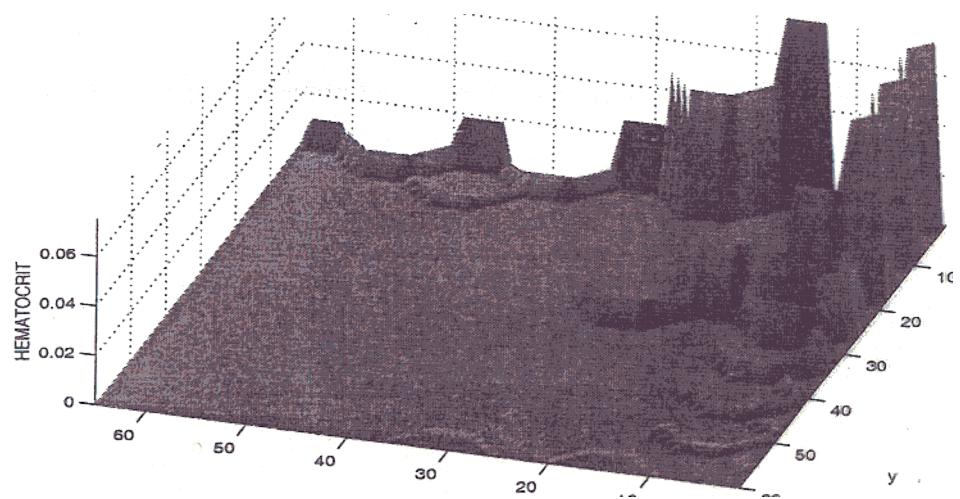
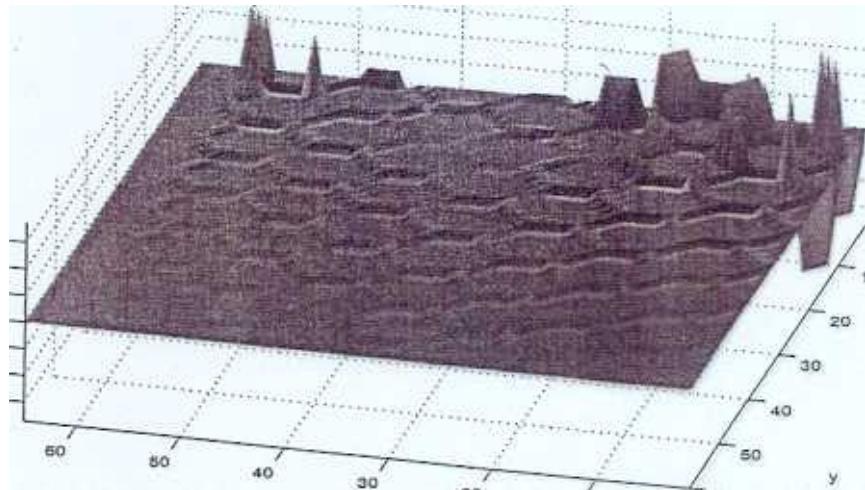
- ①  $\Delta P$   $H_T$  prescribed

$$Q = \frac{\Delta P}{z} \quad (z = \frac{8\mu(H,R)L}{\pi R^4})$$

$\Rightarrow$  flow rate

- ② Given initial network configuration compute flow rates through and pressure drops across each vessel using Krichhoff's Law
- ③ Compute distribution of haematocrit
- ④ Update radius of each vessel
- ⑤ Compute viscosities (using  $H$  and  $R$  from ③ and ④ resp.)
- ⑥ Repeat until steady state reached

## Results



**Figure 4:**

## Automaton Rules

①  $O_2$  distribution determined by BVP

?  $\epsilon$ 's at prob = d d a m e

③ Normal cell if  $O_2 <$  threshold cell dies

> threshold cell attempts to divide

threshold =  $N_{T_1}$  if more normal than cancer neighbours

=  $N_{T_2}$  Cancer normal

$$N_{T_2} > N_{T_1}$$

④ Cancer cell if  $O_2 >$  threshold cell attempts to divide

threshold =  $C_T$  if more cancer than normal neighbour

$C_{T_2}$  normal cancer

$$C_{T_2} > C_{T_1}$$

⑤ Cancer cell if  $O_2 <$  threshold  $\rightarrow$  cell becomes quiescent

If it remains quiescent for a certain length of time  $\rightarrow$  die.

are sinks of  $O_2$

- ⑦ If  $O_2$  level  $\sim$  such that a cell can divide, sample neighbourhood for space  
If more than one available space, go to the one with largest  
If no space die  $\rightarrow$  (Kansal et al 2000) Pater et al 2000

### $O_2$ distribution

$$D_p \nabla^2 P - k(x)P = 0 \quad (\text{adiabatic approx.})$$

$P$   $O_2$  conc

$k(x)$   $k_N$  for normal cell  
 $k_C$  for cancer cel  
 $O$   $O_w$

$$\text{BC} - D_{p,n_w} \nabla P = P(P_b, P) \quad n_w = \text{normal to vessel wall}$$

$P_b$   $O_2$  level in blood  
 $P$  permeability

$$n \cdot \nabla P = 0 \quad (\text{at edge of domain no flux})$$

## Cell Dynamics

$N \times N$  automaton elements

State vector has 3 components

Occupation    normal cell    cancer cell/vessel/empty

Cell status    proliferative/quiescent

Local  $O_2$  conc

We assume for simplicity vessel structure does not evolve

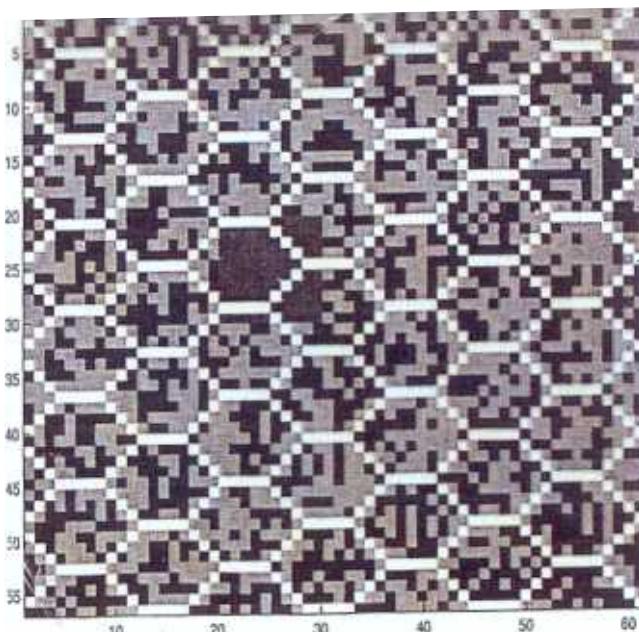
# Parameters

Parameter	Value	Units	Source
$k_m$	0.83	$s^{-1}$	Pries et al (1998)
$Q_{ref}$	40	, nl/min	Pries et al (1998)
$k_s$	1.79	$s^{-1}$	Pries et al (1998)
$\alpha$	0.5	none	Fung (1993)
THR	2.5	none	Fung (1993)
$D_P$	$2.41 \cdot 10^{-5}$	$cm^2 s^{-1}$	Goldman and Popel (2000)
$K_N$	$1.57 \cdot 10^{-4}$	$ml O_2 ml^{-1} s^{-1}$	Goldman and Popel (2000)
$K_T$	$1.57 \cdot 10^{-4}$	$ml O_2 ml^{-1} s^{-1}$	estimated
$\mathcal{P}$	$3.0 \cdot 10^{-4}$	$cm s^{-1}$	estimated
$N_{T1}$	$4.5 \cdot 10^{-4}$	grams	Patel et al (2001)
$N_{T2}$	$4.5 \cdot 10^{-3}$	grams	
$C_{T1}$	$1.5 \cdot 10^{-5}$	grams	
$C_{T2}$	$4.5 \cdot 10^{-5}$	grams	

$$\frac{P_G}{P} = \frac{M_{O_2}}{M_G} \quad m = \text{molecular wt}$$

$m = \text{molecular wt}$

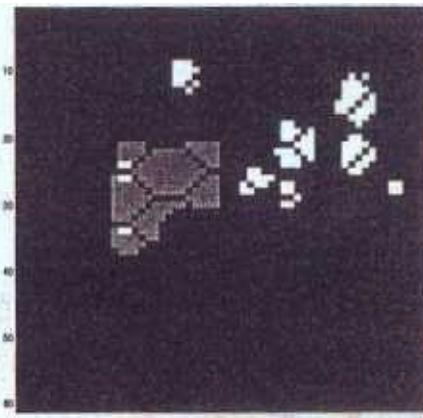
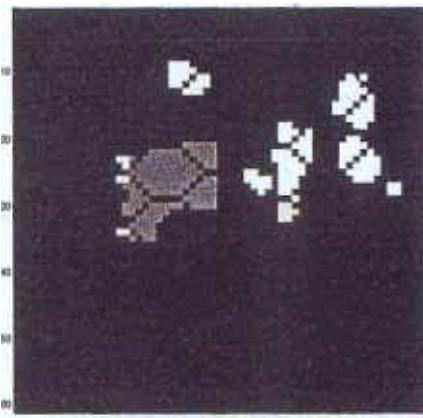
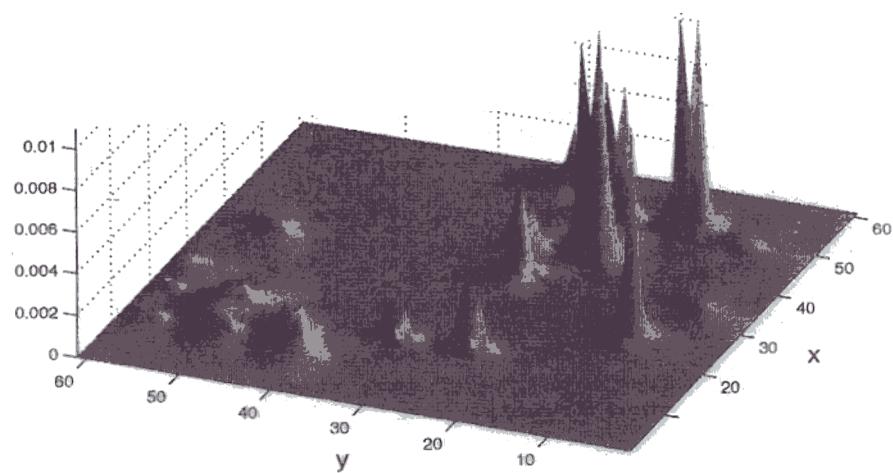
$G = \text{glucose}$  (Patel et al 2001)



### Invasion Dynamics

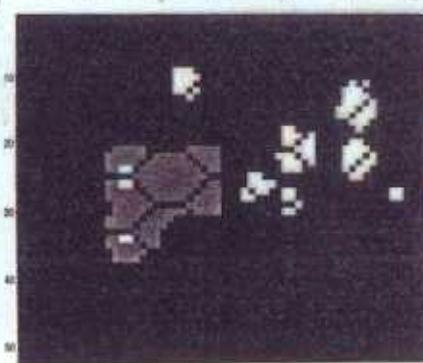
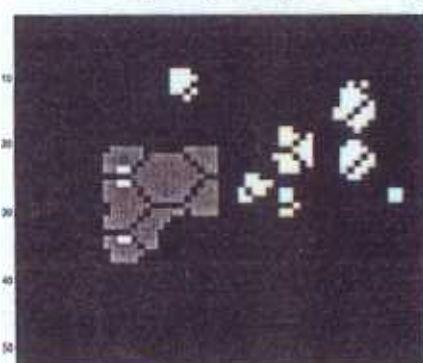
- empty
  - dark grey - cancer
  - light grey - normal
  - Blood vessels
- Heterogeneous

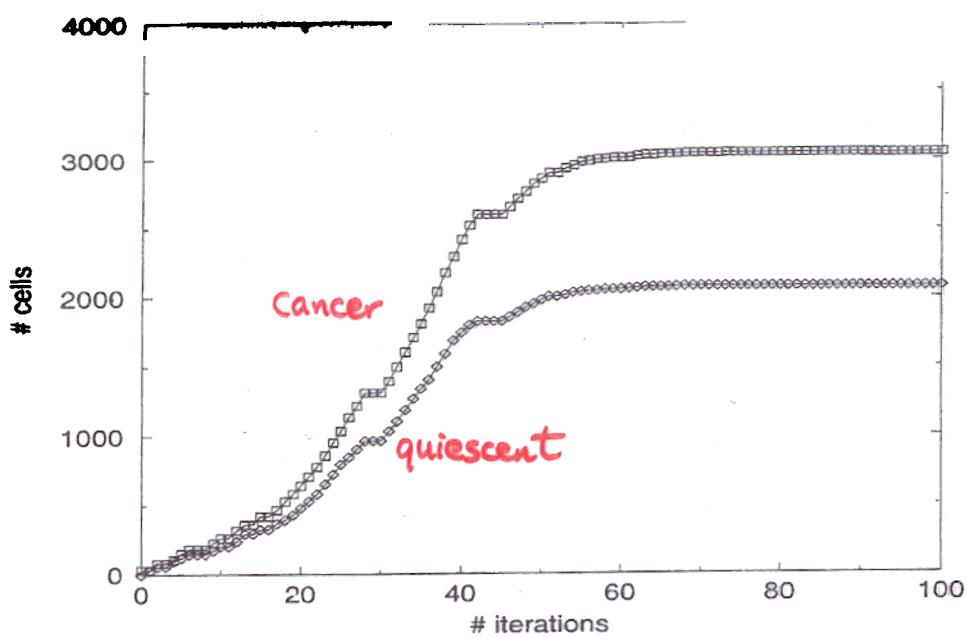
O<sub>2</sub> distribution <sup>P</sup>



### Invasion dynamics

- normal
- empty or blood vess
- grey - cancer

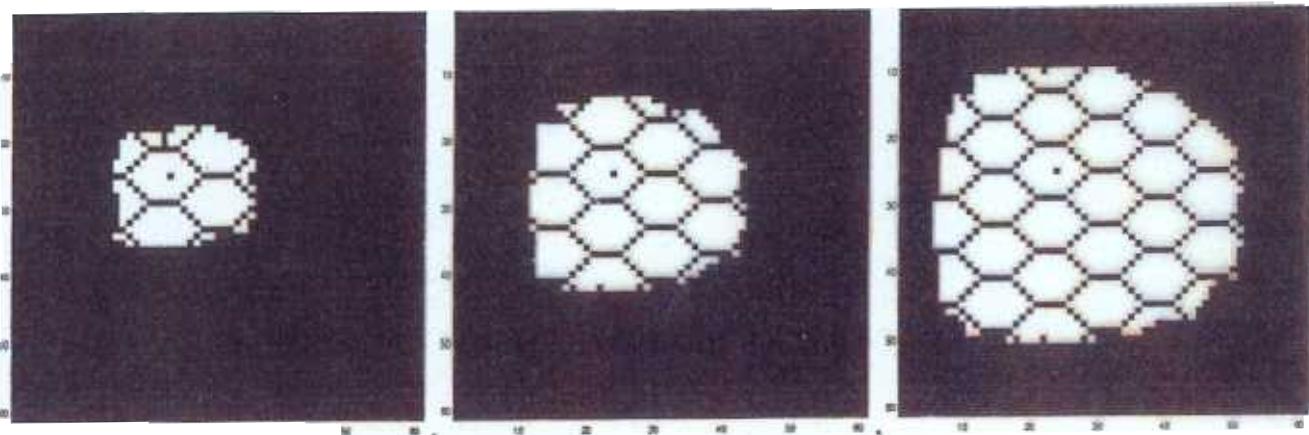
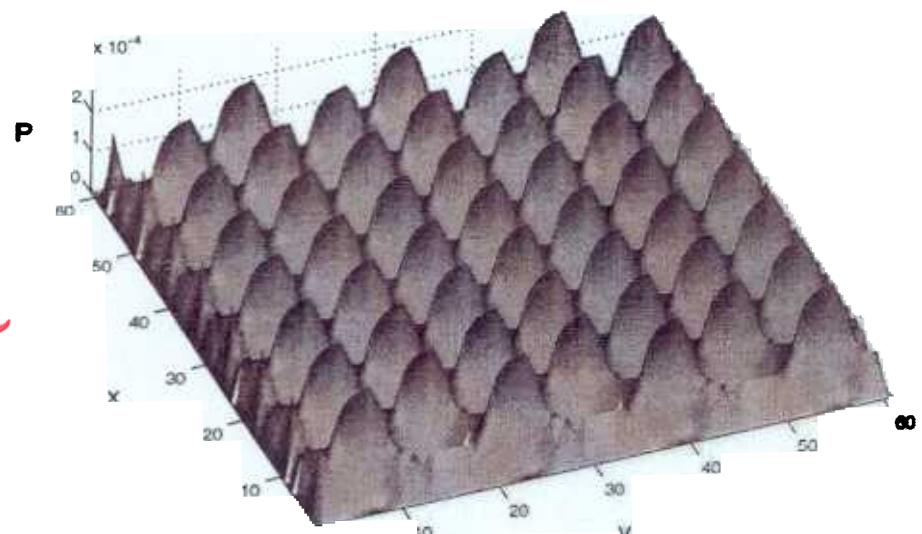




Corresponding homogen case

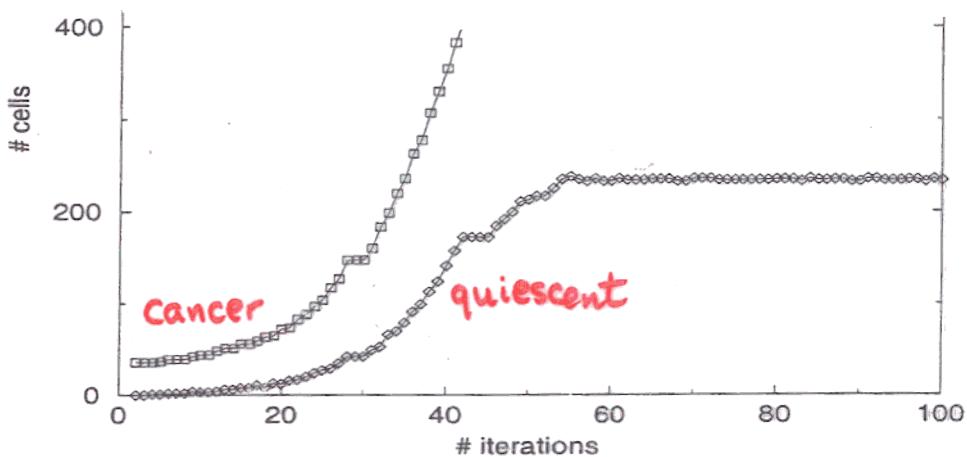
normals  $\downarrow 0$

O<sub>2</sub> distribution



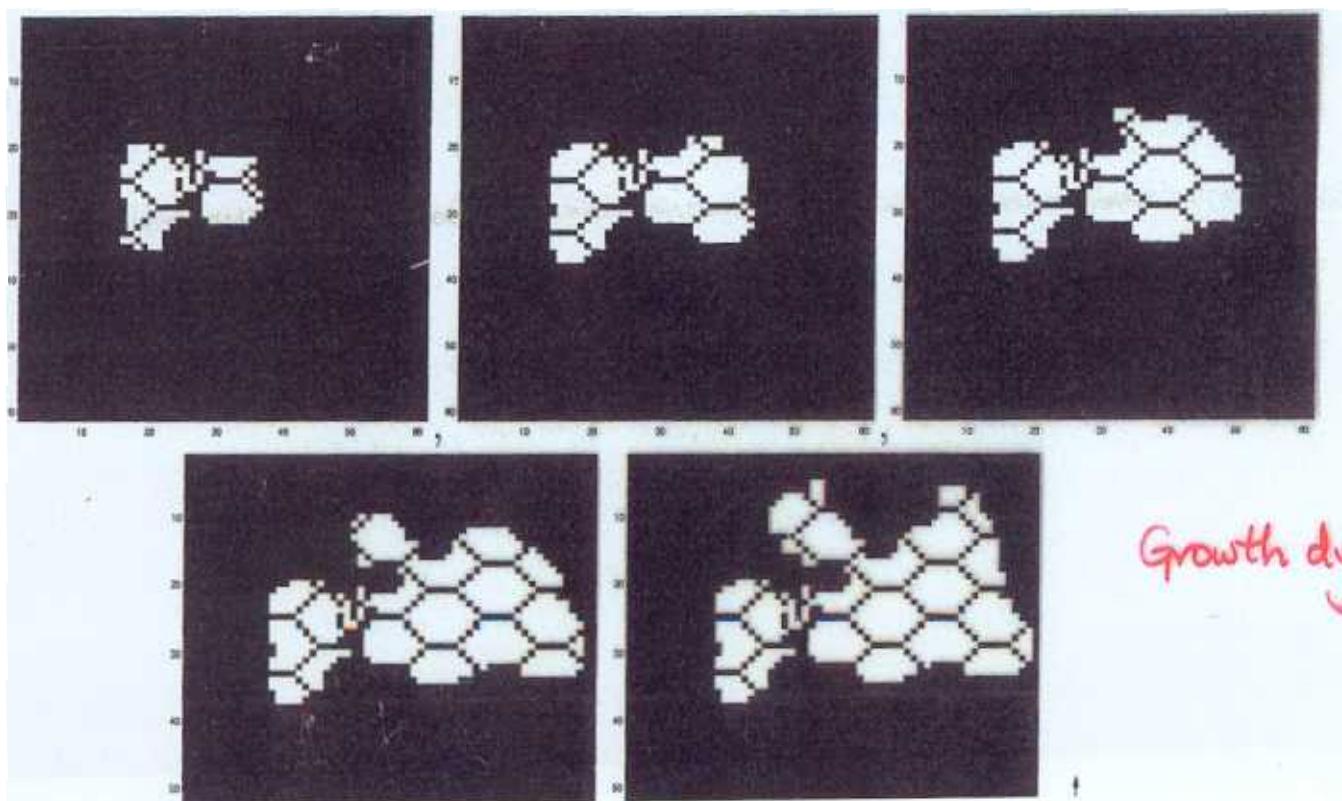
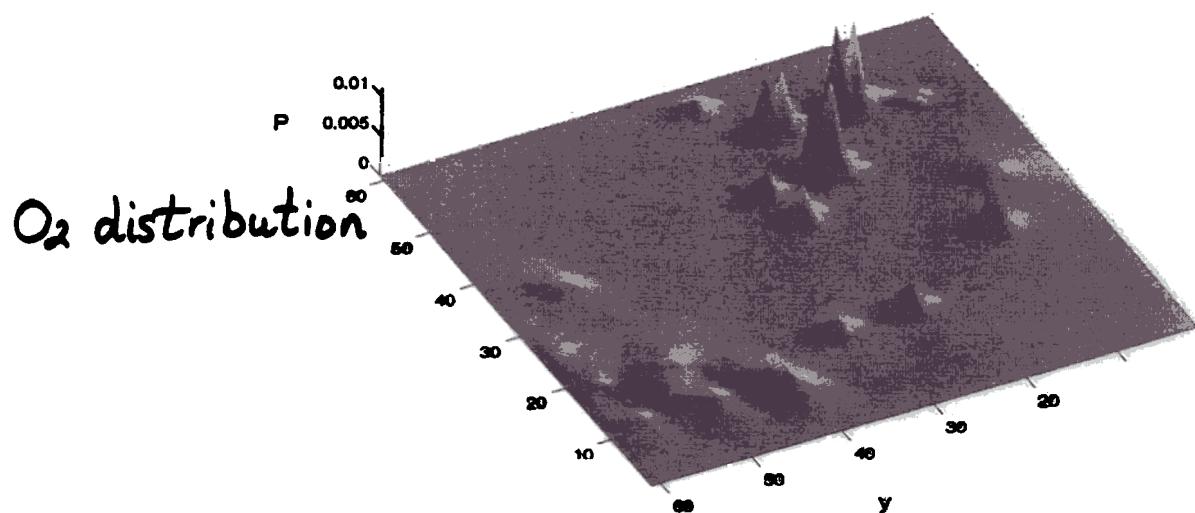
Growth dynamics

## Results



Heterogeneous Case

normals  $\downarrow 0$



Growth dynamics

- \* Environmental heterogeneity restricts dramatically the ability of malignant colonies to invade healthy tissue

## Cell-Cycle Dynamics

- Why ?

nutrient demand

hypoxia-induced quiescence

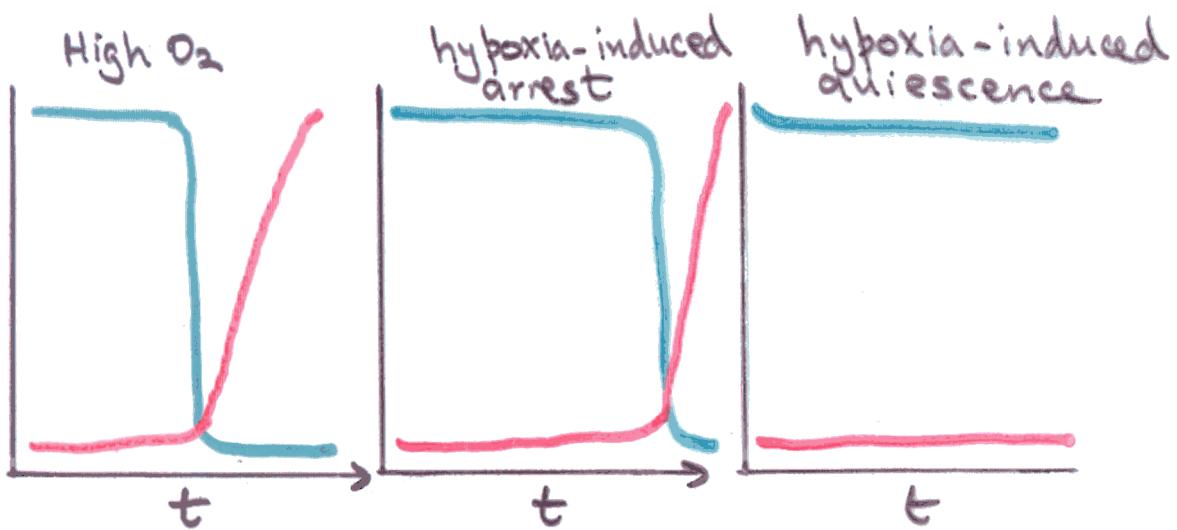
drugs work only on cells in a certain part of their cell cycle.

Cell Cycle       $G_1$      $S G_2$

cyclin-dependent kinases (CDK) }  
cyclins } 2 families of proteins

In  $G_1$ , CDK activity slow because its cyclin partner are missing.

At Finish Cdk1 (and Cdc20) concs are high  
degrade cyclins



Cdhl-APC —

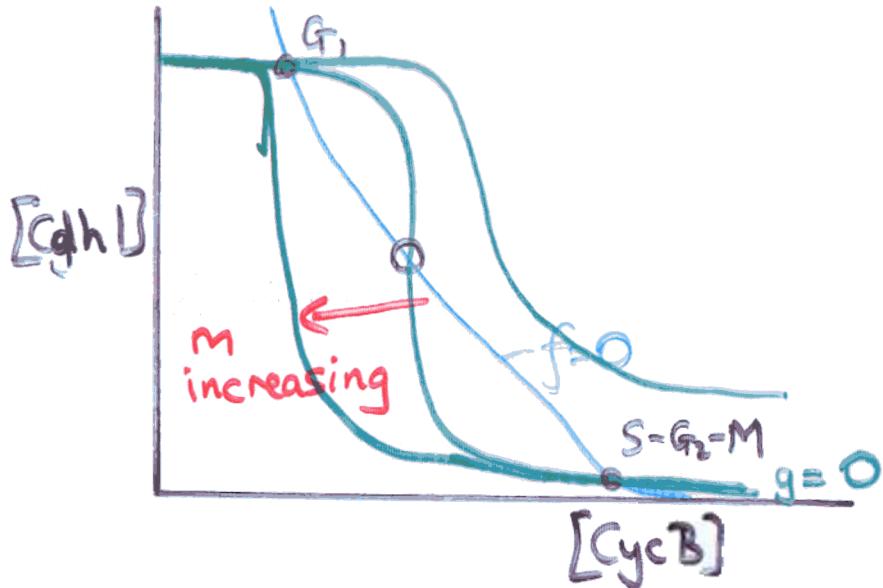
Cyc-CDK —

$$\frac{d}{dt} [\text{CycB}] = f([\text{CycB}], [\text{Cdhl}])$$

$$\frac{d}{dt} [\text{Cdhl}] = g([\text{CycB}], [\text{Cdhl}], m)$$

mass of cell

Tyson & Novak



$$\frac{dm}{dt} = k \left(1 - \frac{M}{M_{\infty}}\right)m$$

This is a model for the G S transition - NOT the cell cycle.

v

# Response to hypoxia (low O<sub>2</sub>)

Expts on mouse embryo fibroblasts

Normal cells  $\xrightarrow{\text{hypoxia}}$  G<sub>1</sub> arrest

Does not occur with p27<sup>nu</sup> mutants

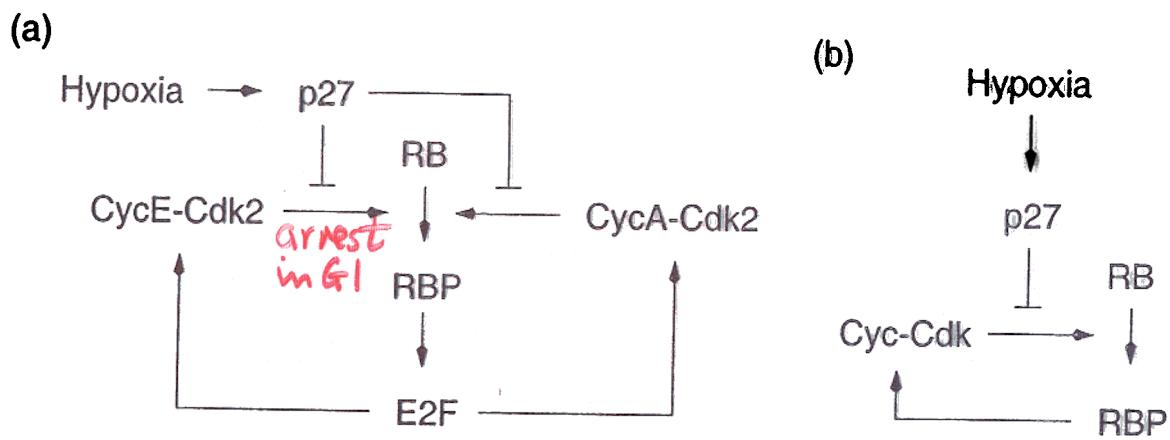


Figure 1: Schematic representation of the mechanism for hypoxia-induced cell-cycle arrest.  
 (a) The original mechanism proposed by Gardner et al (2001). (b) Our simplified version for modelling purposes. RBP stands for the phosphorylated form of the RB protein.

*E2F - transcription factor*

Take Tyson & Novak model:

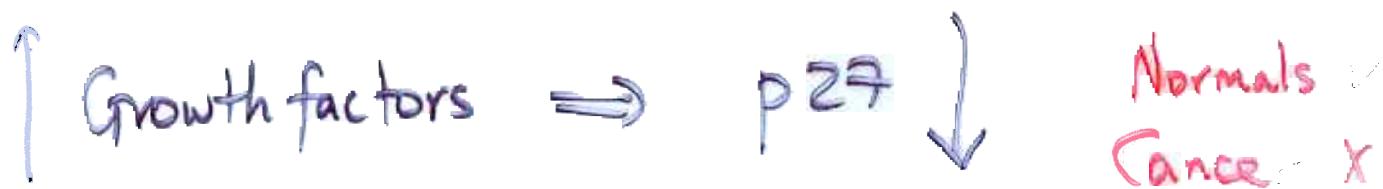
Incorporate inhibition by a  $-k_2 z$  term  
 $\uparrow$   
 p27 conc. in (dih)

$$\frac{dz}{dt} = k_1 \left(1 - \frac{m}{m_x}\right) - k_2 \frac{P}{B+P} z \quad \begin{matrix} \text{oxygen} \\ \text{growth regulation} \\ \text{[as } m \uparrow z \downarrow] \end{matrix} \quad \begin{matrix} \text{Normals} \\ \text{hypoxia} \end{matrix}$$

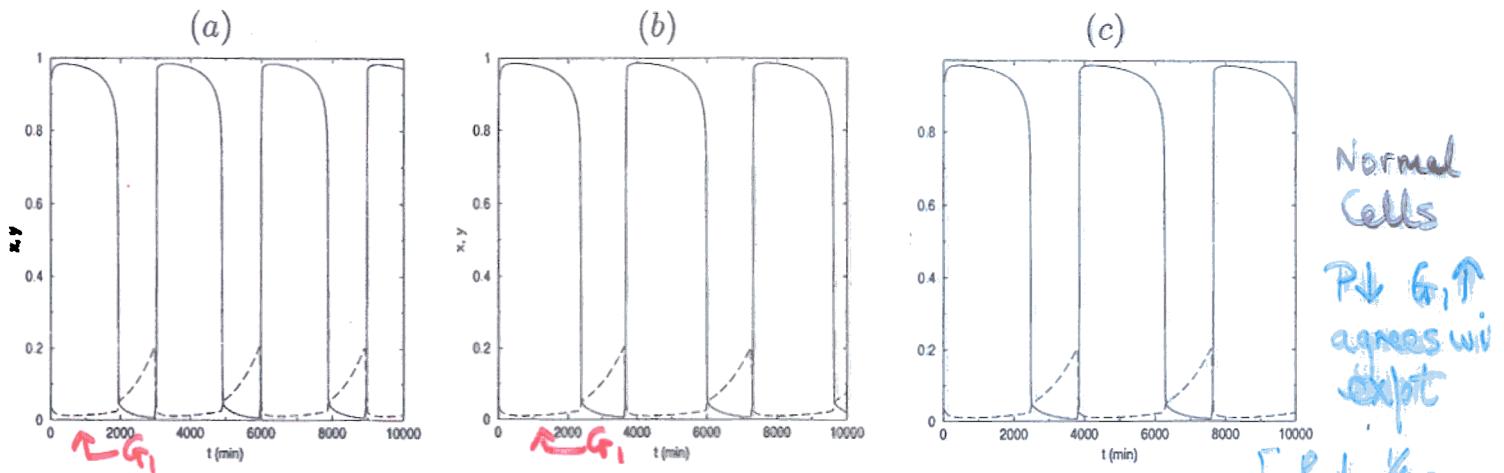
$$\frac{dz}{dt} = k_1 - \frac{k_2 P}{B+P} z \quad \begin{matrix} \text{Cancer} \\ \text{Cells} \end{matrix}$$

Hypothesis - growth regulation +  
 is lost

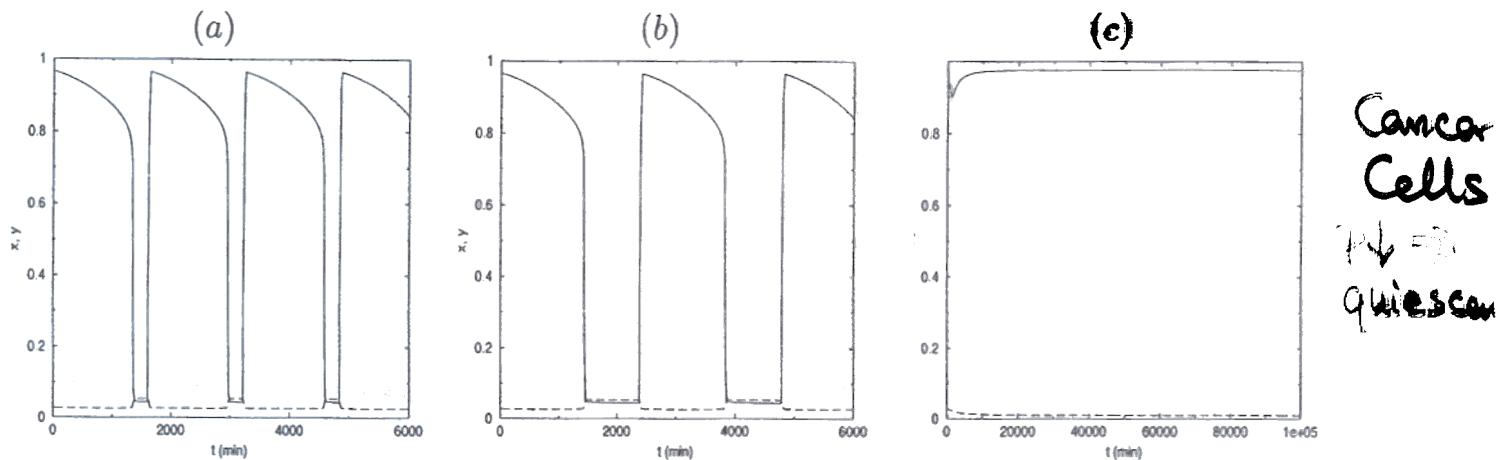
## Growth regulation of p27?



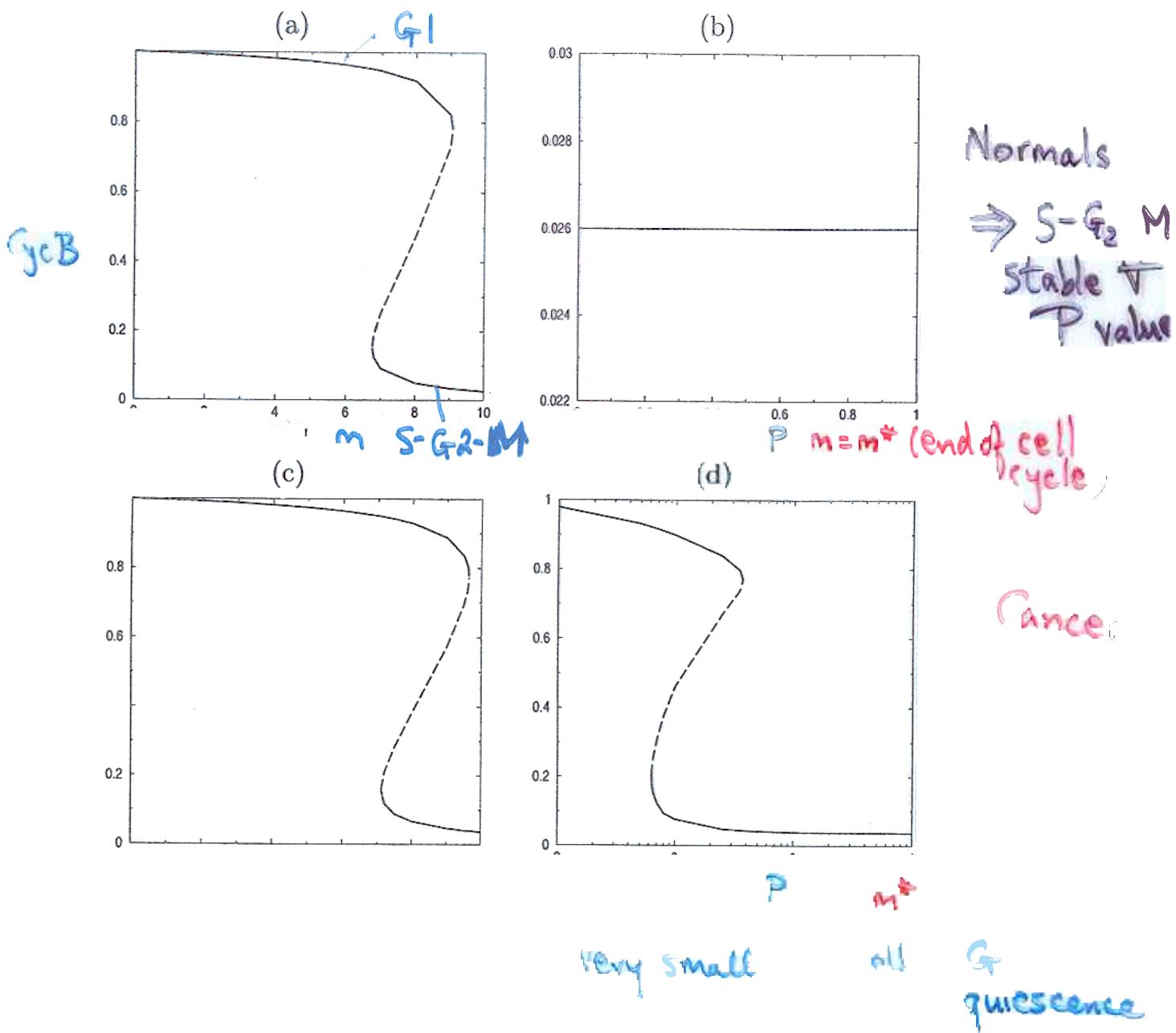
If growth is arrested, p27 is upregulated

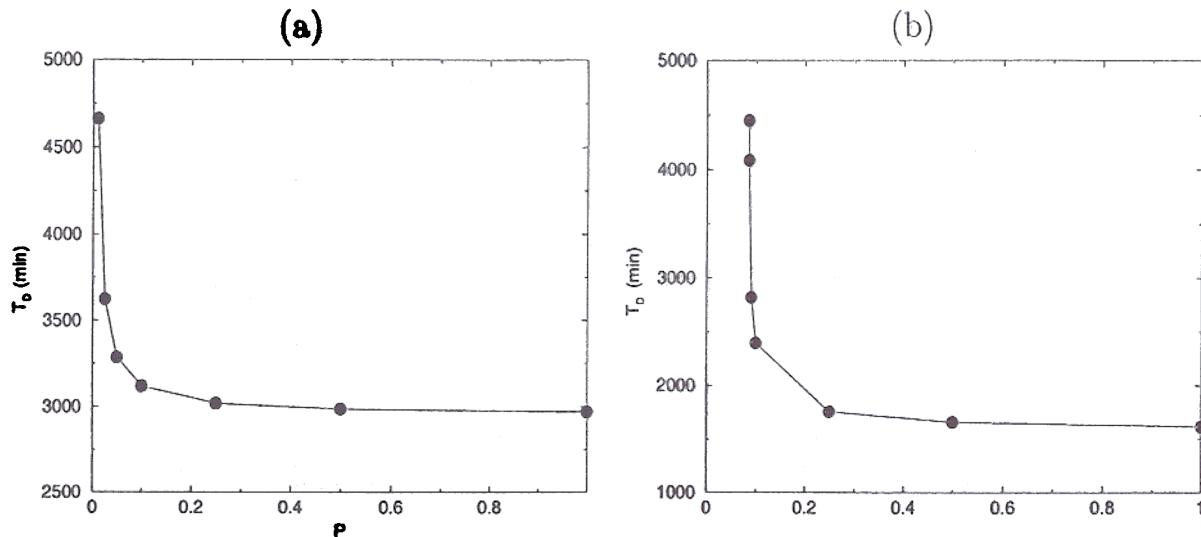


**Figure 2:** Numerical solutions of the system Eqs. (5)-(6) for different values of the oxygen tension  $P$ : (a)  $P = 1$ , (b)  $P = 0.025$ , (c)  $P = 0.02$ . Solid lines correspond to  $x$  and dashed lines to  $y$ . The parameter values used in this simulations are shown in Table 1.



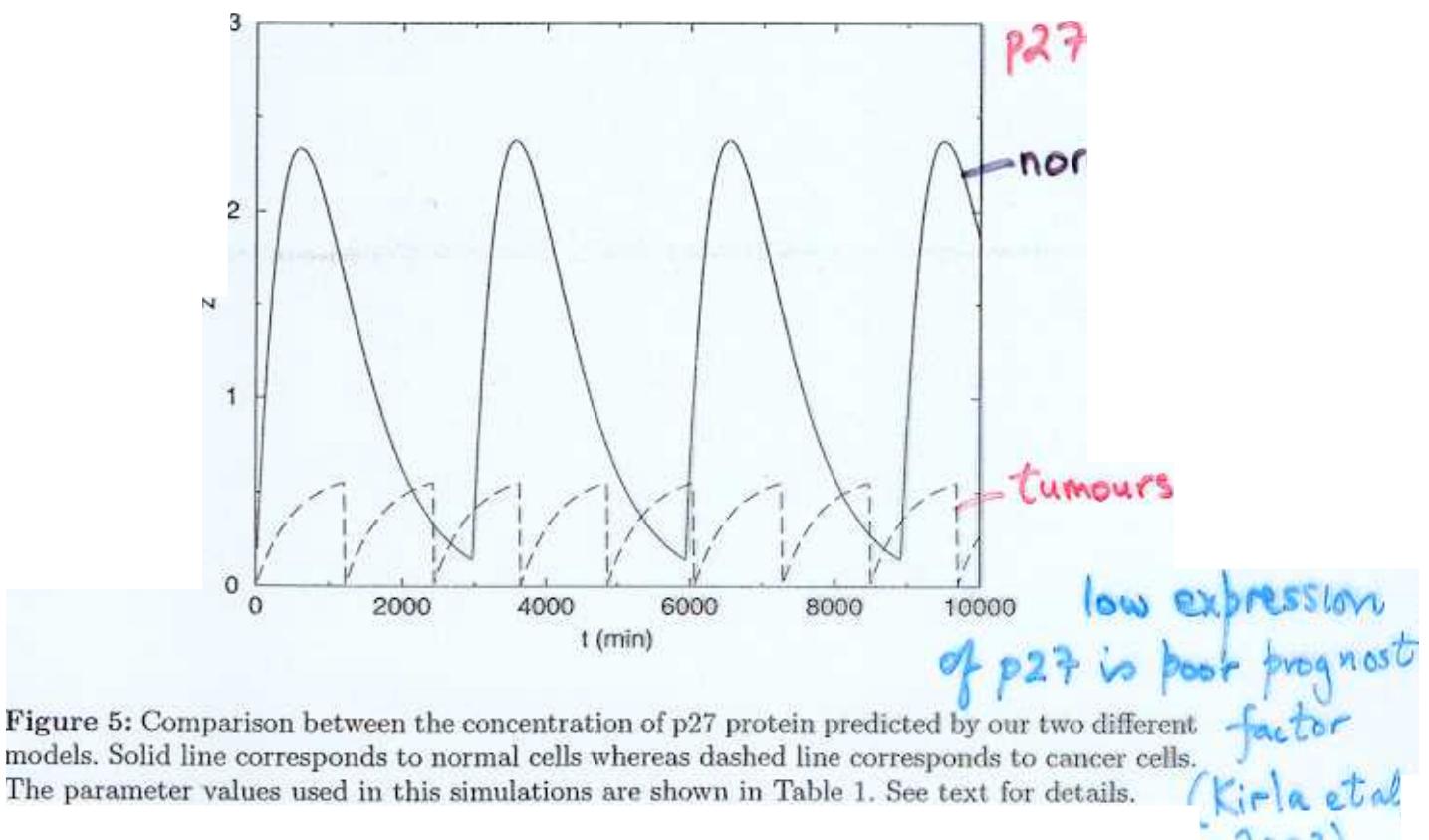
**Figure 3:** Numerical solutions of the system Eqs. Eqs (4)-(6) and (9)-(10) for different values of the oxygen tension  $P$ : (a)  $P = 1$ , (b)  $P = 0.1$ , (c)  $P = 0.01$ . Solid lines correspond to  $x$  and dashed lines to  $y$ . The parameter values used in this simulations are shown in Table 1.





**Figure 4:** Division time as a function of the oxygen tension,  $P$ . (a): normal cells, (b): cancer cells. Note the vertical asymptote in (b) at  $P \simeq 0.085$ , which is the critical value of the oxygen tension for the transition to quiescence in cancer cells. The parameter values used in this simulations are shown in Table 1.

concentration of p27 increases as  $k_5/k'_5$  increases. Also, the division time is an increasing function of  $k_5/k'_5$ . However in this case we do not observe any divergence in  $T_D$ , which confirms that quiescence cannot be induced in this model.



**Figure 5:** Comparison between the concentration of p27 protein predicted by our two different models. Solid line corresponds to normal cells whereas dashed line corresponds to cancer cells. The parameter values used in this simulations are shown in Table 1. See text for details.

(Kirla et al  
2001)

## Possible Application

Doxorubicin treatment of non-Hodgkin's lymphoma  
(Ben Kibba, Ezra Agur, Tomas Alarcon, PKM)  
K. Marron

Structural adaptation

Vessels surrounded  
by NHL  $\Rightarrow$  leaky & unstable

Nutrient diffusion

drug pharmacokinetics in plasma  $\frac{dc}{dt}$   $\propto k_c$   
pharmacodynamics  $k_{lls}$  kills proliferating cells  
tissue dynamics adiabatic approx.

AIM Explore different protocols of treatment  
(presently a 2 day cycle is employed)

## CONCLUSION

- \* heterogeneities have a profound effect on tumour dynamics
  - effects of p27 possible mechanism
- \* efficiency of drug treatments

## Future Directions